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# Electrical Response and Thermal Damage Assessment of Cutaneous and Subcutaneous Tissues to Noninvasive Radiofrequency Heating: A Computational Modeling Study

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**1. Introduction**

**2. Mathematical modeling**

**3. Results**

**4. Conclusions**

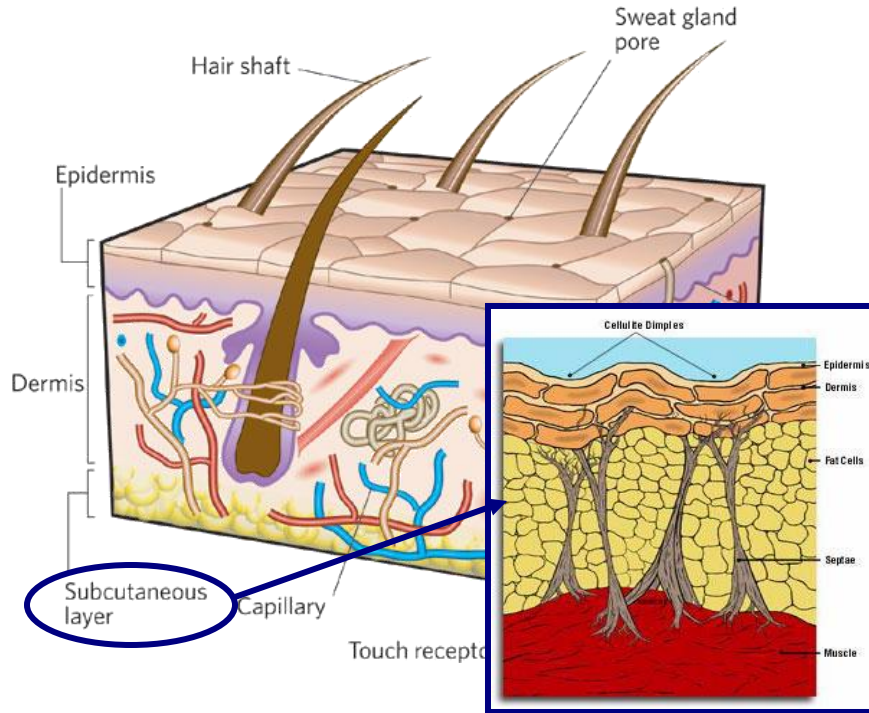
## **1. Introduction**

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## □ Skin-fat structure



- **Epidermis**: outer cellular layer (~0.1 mm)
- **Dermis**: A dense connective tissue layer perfused with micro-vessels (~1 mm)
- **Hypodermis** (or **subcutaneous tissue**): a fine, collagenous and fibrous septa network with clusters of fat cells (1 cm to 10 cm)

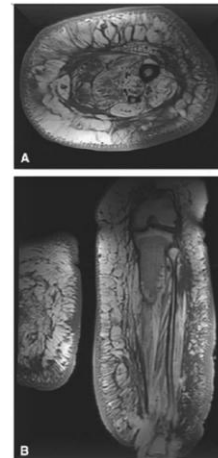
## □ Radiofrequency (RF) heating

A **non-invasive** technique can be used to produce **selective heating** of subcutaneous tissue



## □ Clinical applications

**Subcutaneous fat diseases:**  
Lipomatosis, Madelung's disease, lipedema or cellulite



## □ Objectives

- Model a real structure of subcutaneous tissue
- Assess the electrical and thermal effect of fibrous septa within subcutaneous tissue during RF hyperthermic heating ( $< 55^{\circ}\text{C}$ )
- Quantify and compare the thermal damage occurred in two subcutaneous tissue structures (one composed by fat only and another by fat and fibrous septa)



**COMSOL Multiphysics 4.3b**

1. Introduction

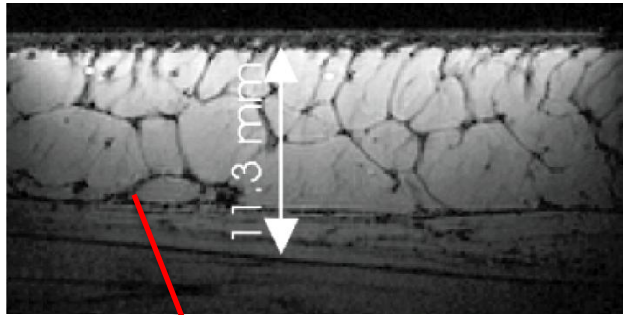
**2. Mathematical modeling**

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## □ Domain Geometry

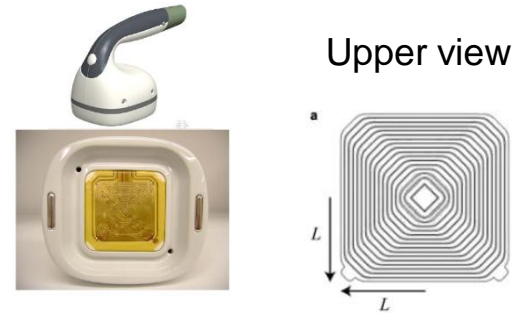
**MRI skin of a female** (Mirrashed, F., et al., *Skin Research and Technology*, 10, 2004).



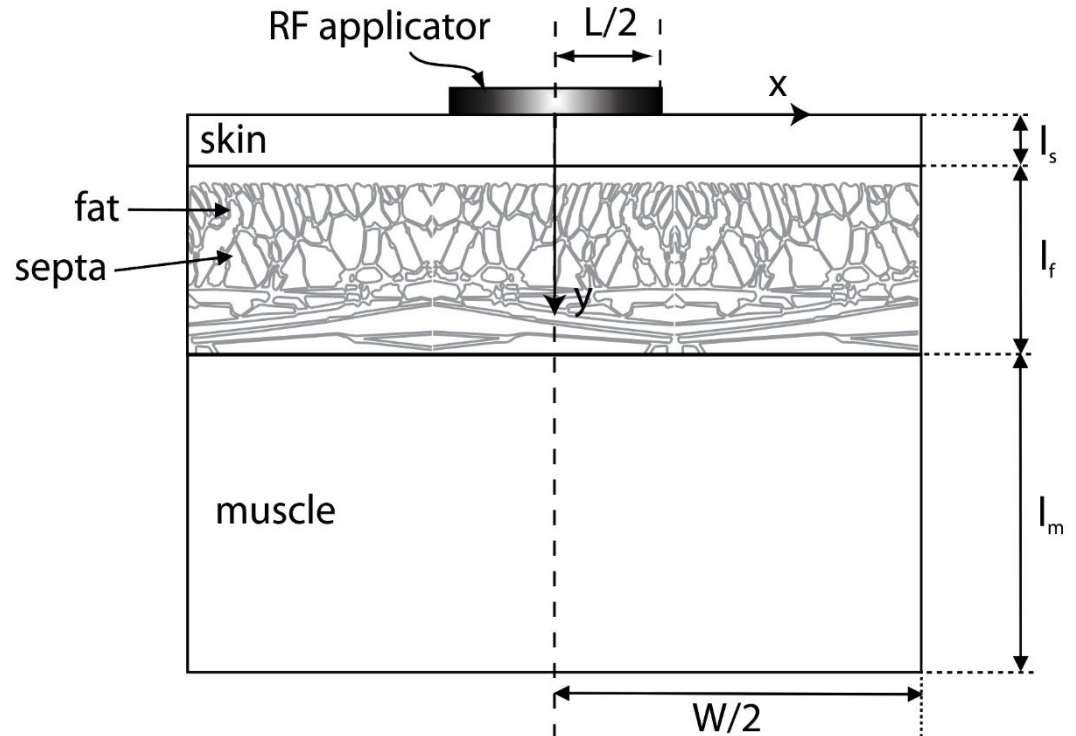
Fibrous septa



**RF monopolar applicator** (Franco, W. et al. *LSM 42*, 2010)



RF applicator



## □ Governing Equations

### □ Coupled electric-thermal problem

#### ① Thermal problem: Heat Transfer

$$\rho c \frac{\partial T}{\partial t} = \nabla(k \nabla T) + Q_m + c_b \omega (T_b - T) + Q$$

$Q = \sigma |E|^2$

#### ② Electric problem: Electric Currents

$$\nabla \sigma \nabla V = 0$$

### □ Thermal damage problem

#### ③ Arrhenius Equation: Domain ODEs and DAEs

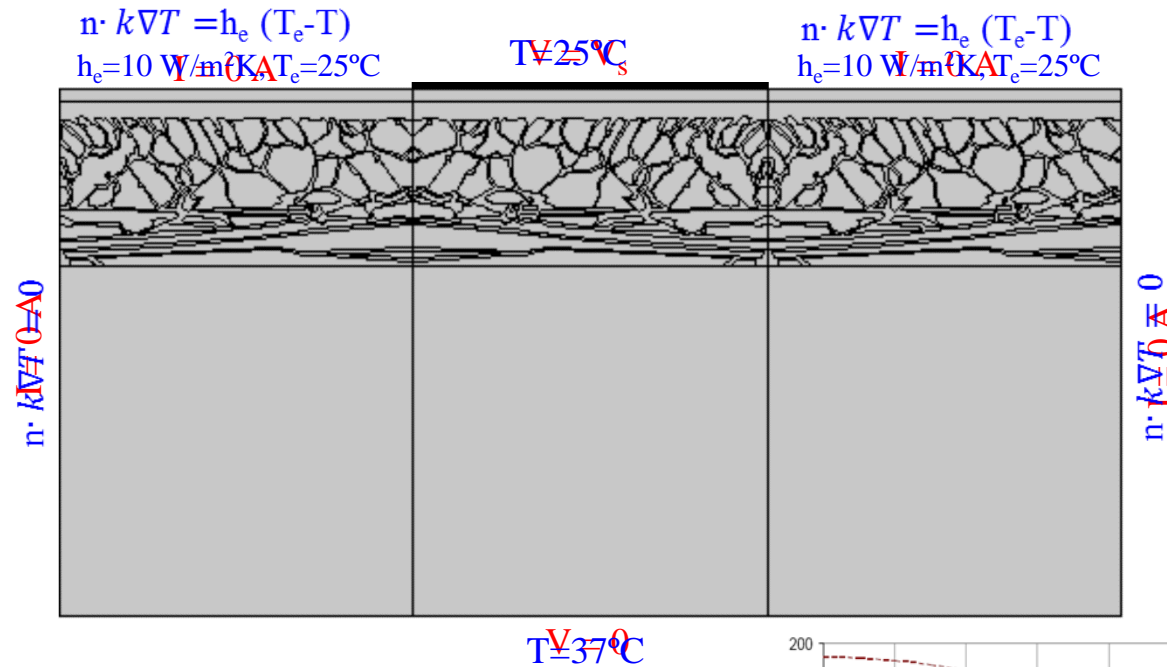
$$\Omega(t) = \int_0^t A \cdot e^{\frac{-\Delta E}{RT}} dt$$

- A and  $\Delta E$  for skin (Weaver and Stoll 1969)
- $\Omega = 1 \rightarrow$  lesion contour (transepidermal necrosis, 63% reduction in cell viability)

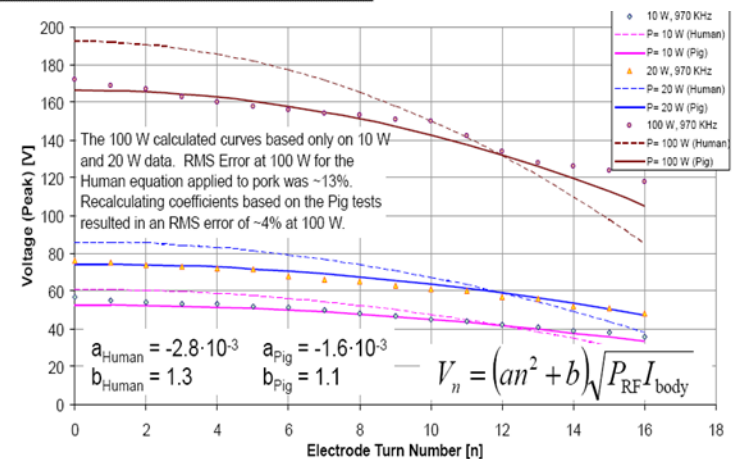


## □ Boundary conditions

## ■ Thermal conditions



$$V_s(-L \leq y \leq L, 0) = \left( a \left( l \frac{y}{L} \right)^2 + b \right) \sqrt{PI}$$



## □ Thermal and electrical characteristics of the model elements

Element	$\epsilon_r$	$\sigma$ (S/m)	$k$ (W/m·K)	$\rho$ (kg/m <sup>3</sup> )	$c$ (J/kg·K)	$\omega$ (kg/m <sup>3</sup> ·s)
Skin	1832.8	0.22	0.53	1200	3800	2
Fat	27.22	0.025	0.16	850	2300	0.6
Muscle	1836.4	0.5	0.53	1270	3800	0.5
Septa	1832.8	0.22	0.53	1200*	3800	0

## □ Main Physical assumptions

- Homogeneous tissues
- Tissues have isotropic electric and thermal properties
- Constant  $k$ ,  $c$  and  $\omega \rightarrow$  variations are not significant within the 35-50°C range
- Properties of the fibrous septa similar to those of the dermis
- The perfusion term in the septa is neglected (i.e. fibrous septa as solid)

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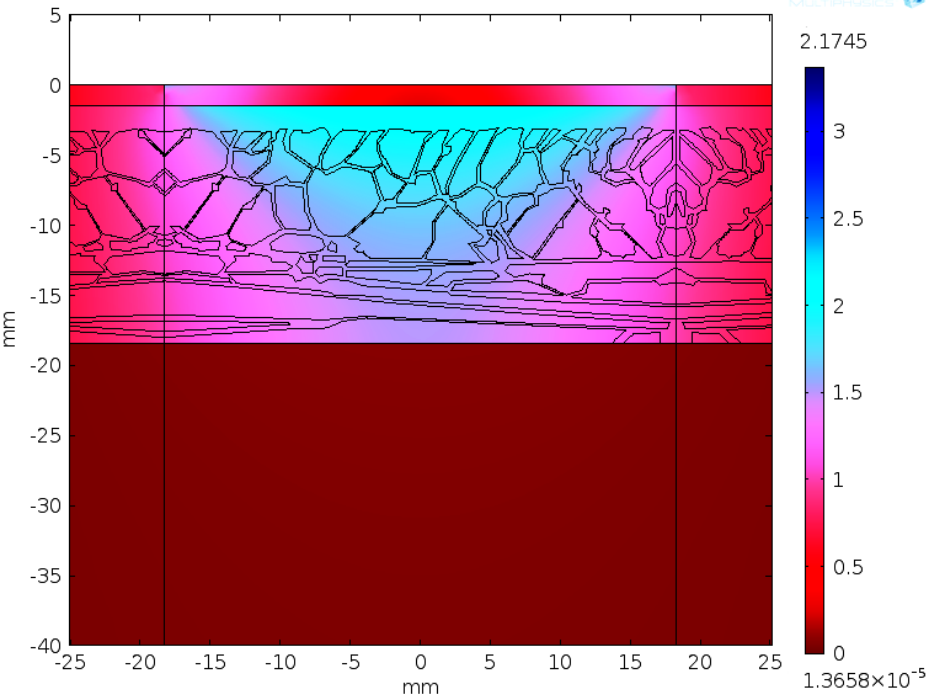
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## □ Electric field

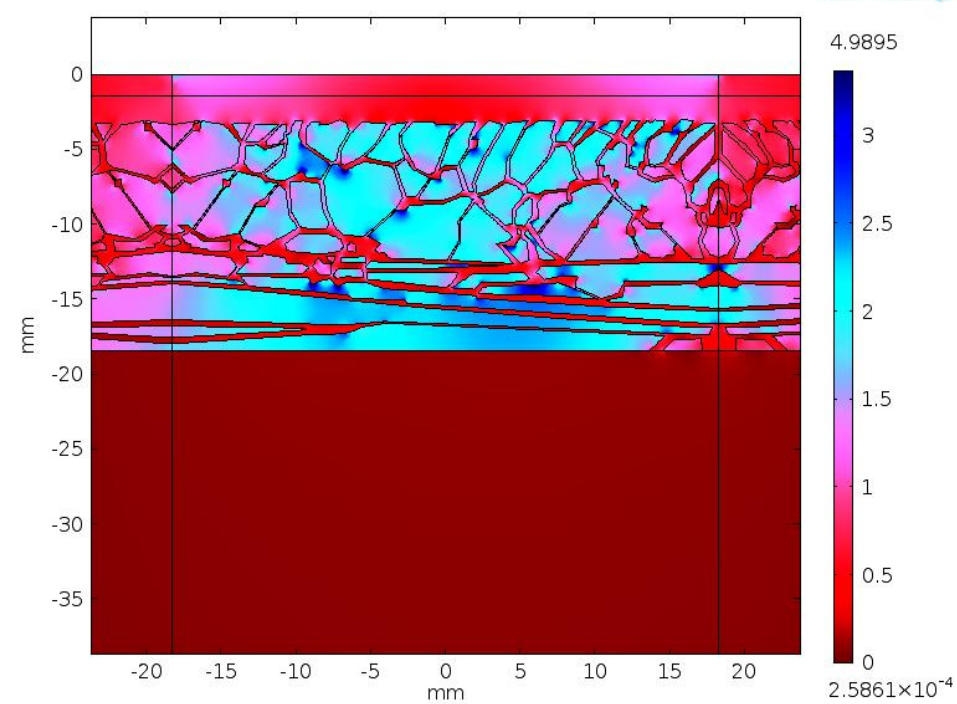
**Subcutaneous tissue with fat only  
(no fibrous septa)**

**Subcutaneous tissue with fat and  
fibrous septa**

Time=2500 Surface: Electric field norm (V/mm)



Time=2500 Surface: Electric field norm (V/mm)

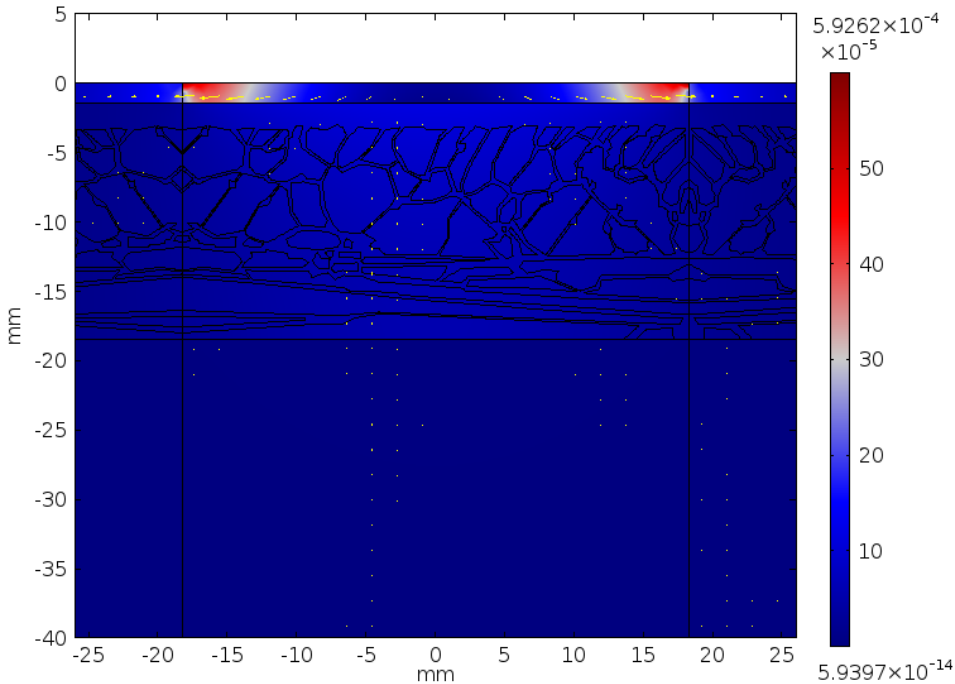


## □ Total electric power absorption (Q) and Electric currents (arrows)

### Subcutaneous tissue with fat only (no fibrous septa)

Time=2500 Surface: Total power dissipation density (W/mm<sup>3</sup>)  
Arrow Surface: Current density (Material)

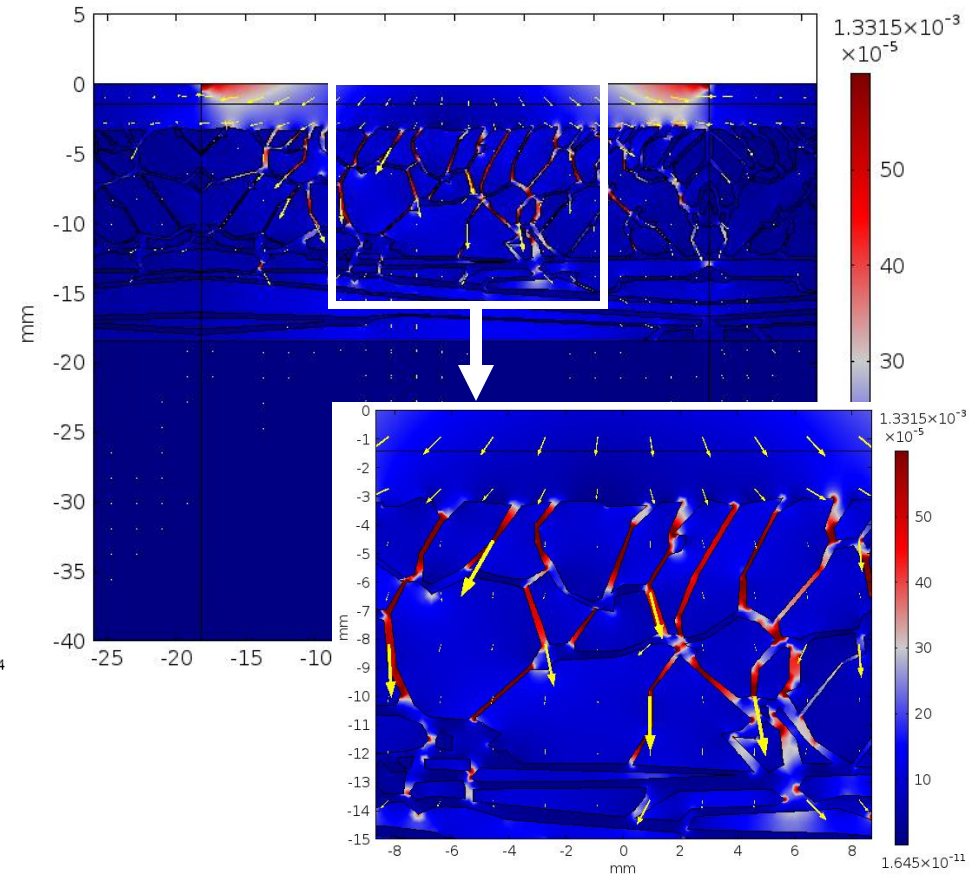
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### Subcutaneous tissue with fat and fibrous septa

Time=2500 Surface: Total power dissipation density (W/mm<sup>3</sup>)  
Arrow Surface: Current density (Material)

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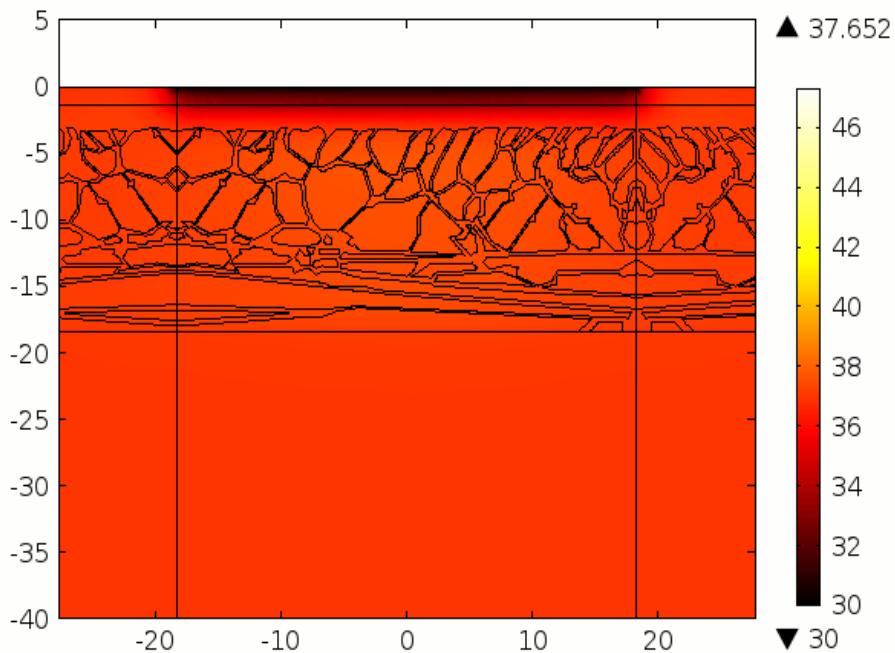


## □ Temperature distribution and thermal damage

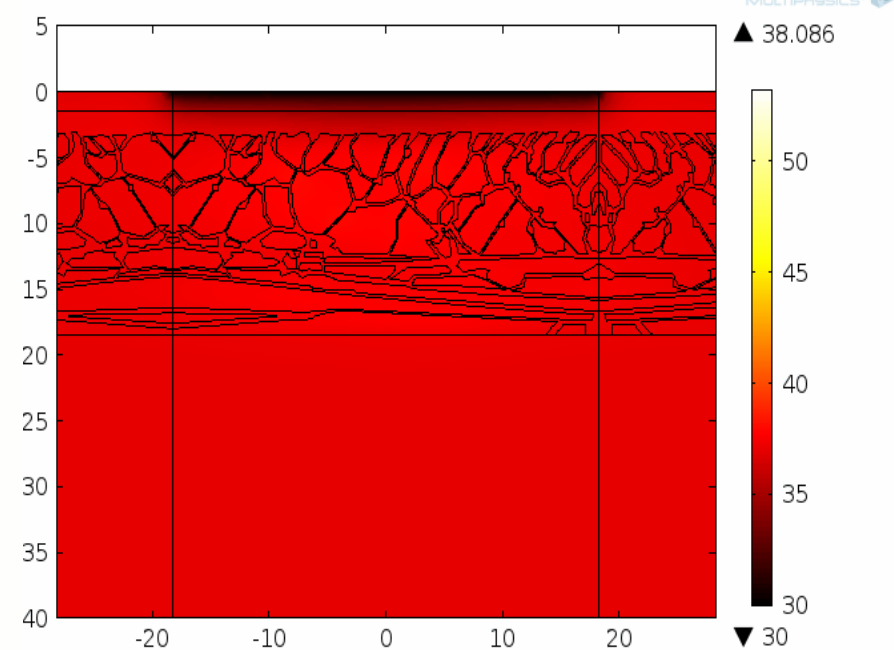
**Subcutaneous tissue with fat only  
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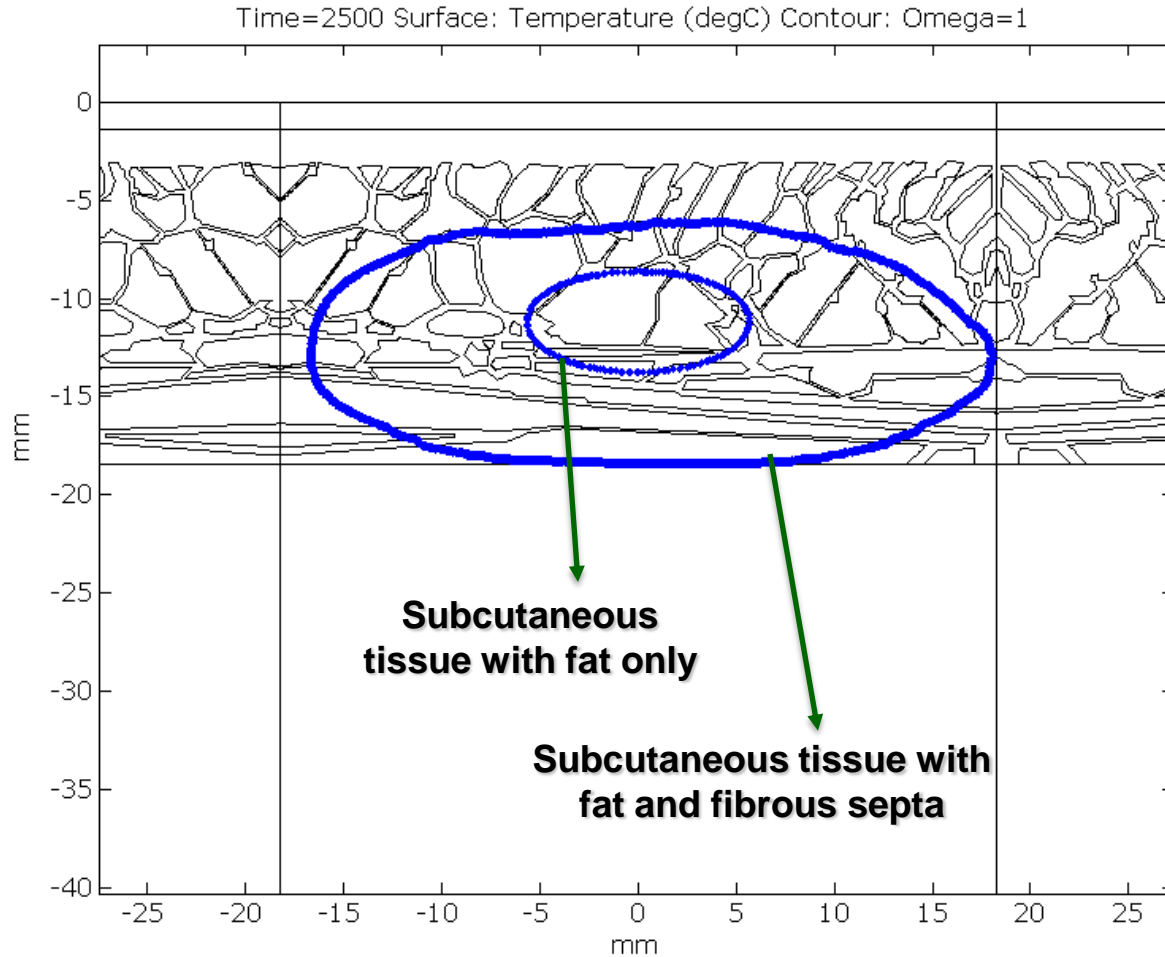
Time=0 Surface: Temperature (degC)



Time=0 Surface: Temperature (degC)



## □ Thermal damage quantification



The lesion volume is ~ 7 times higher considering fibrous septa

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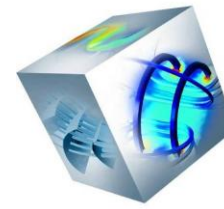
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- ❑ Our results demonstrate the **importance** of including the fibrous septa when modeling RF heating of subcutaneous tissue:
  - ❑ The intensity and extent of the electric field in the subcutaneous tissue is increased considering fibrous septa network
  - ❑ Fibrous septa favors the flux of electric current → increasing the intensity of the electric field, which in turn increases power absorption within subcutaneous tissue
  - ❑ Neglecting the electric and thermal energy contributions of the fibrous septa results in underestimating thermal damage
  
- ❑ Our findings would be **useful** to design and develop novel devices and treatments to subcutaneous fat diseases during RF hyperthermic heating



**Knowledge of correct dosimetry**



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