



# EUROPEAN COMSOL CONFERENCE 2010

Paris November 17-19, 2010

## FROM CT SCAN TO PLANTAR PRESSURE MAP DISTRIBUTION OF A 3D ANATOMIC HUMAN FOOT

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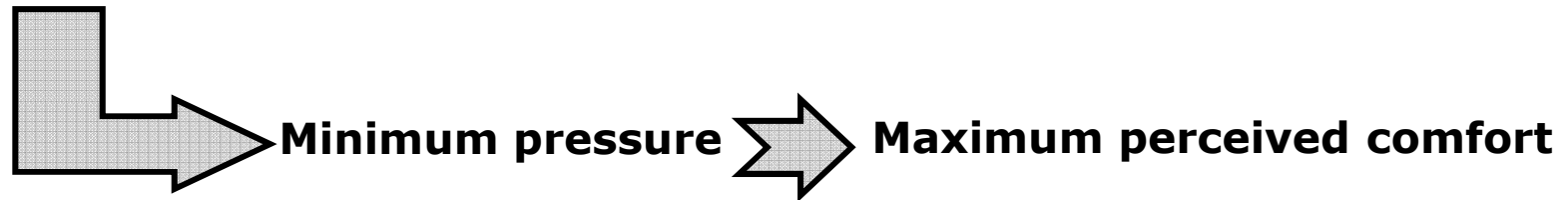
University of Molise  
School of Engineering - Italy

# Outline

- Introduction and Aims
- From CT images to numerical results
  - ✓ CAD modeling
  - ✓ FE modeling (non-linear material law, contact analysis)
- Numerical Issues
- Result Analysis
- Final Remarks

# Introduction and Aims

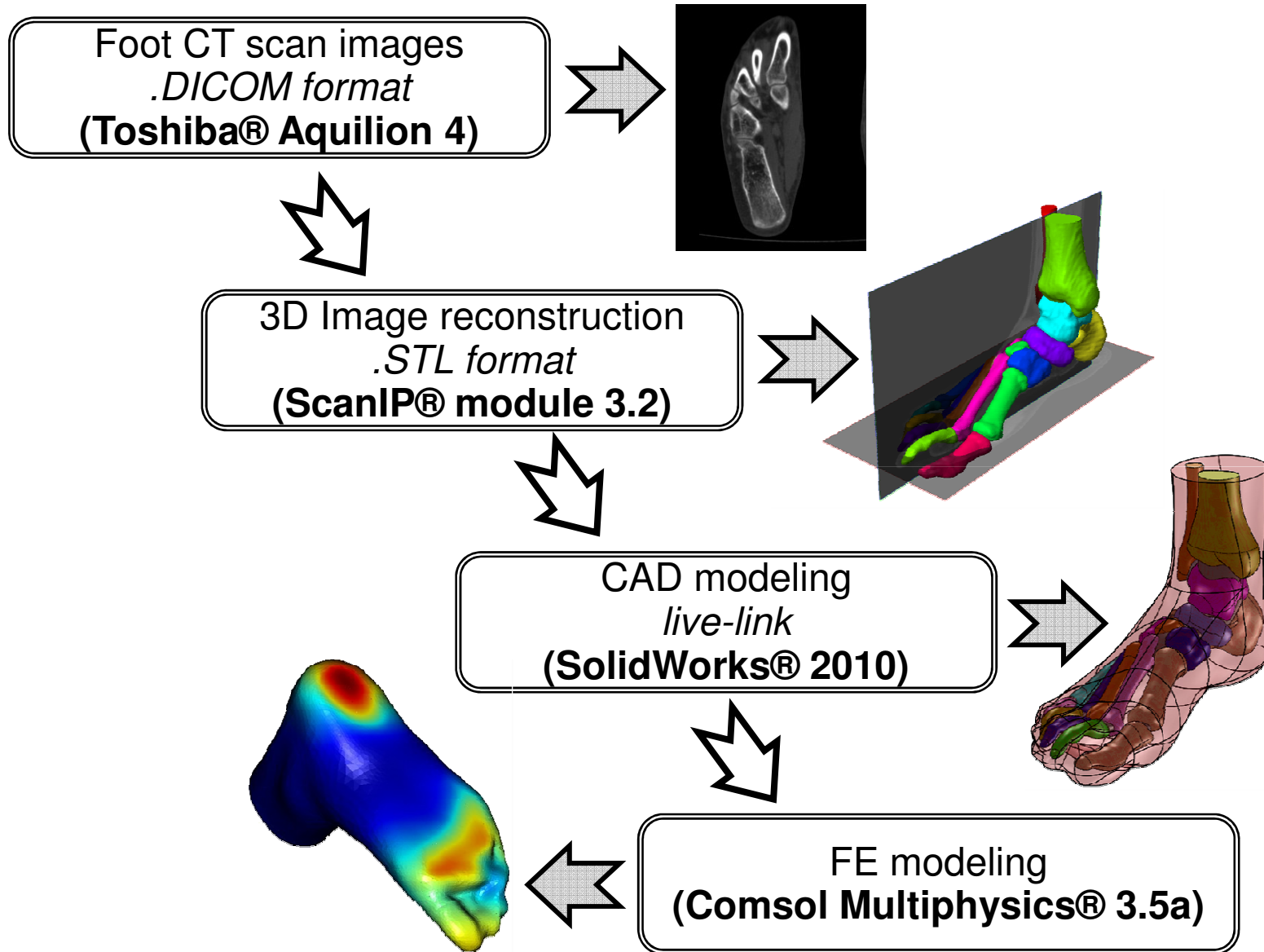
- ❑ Stress-strain behavior of human foot tissues and pressure map distributions at the plantar interface are of interest
- ❑ Plantar pressure maps highly influence perceived **human comfort** at insole footwear interface.



## ... in this work

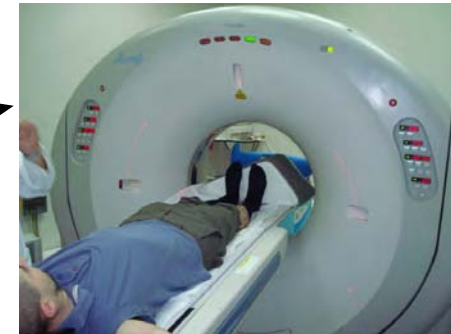
- ❑ Building-up 3D human foot model into **Comsol Multiphysics® 3.5a**
- ❑ Facing out numerical issues:
  - ✓ *Non-linear materials*
  - ✓ *Contact analysis*
  - ✓ *Large deformation*

# Methodology Overview

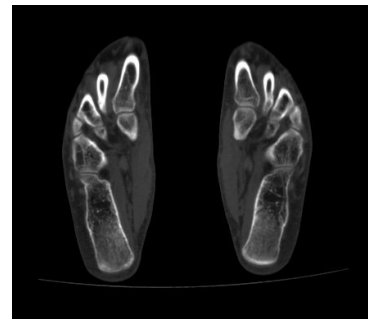


# Methodology Overview

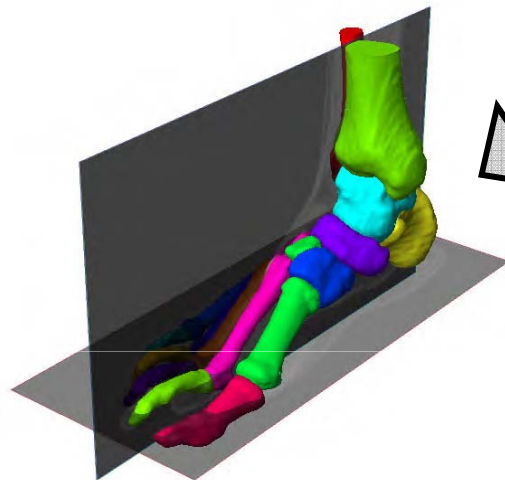
## Image Processing



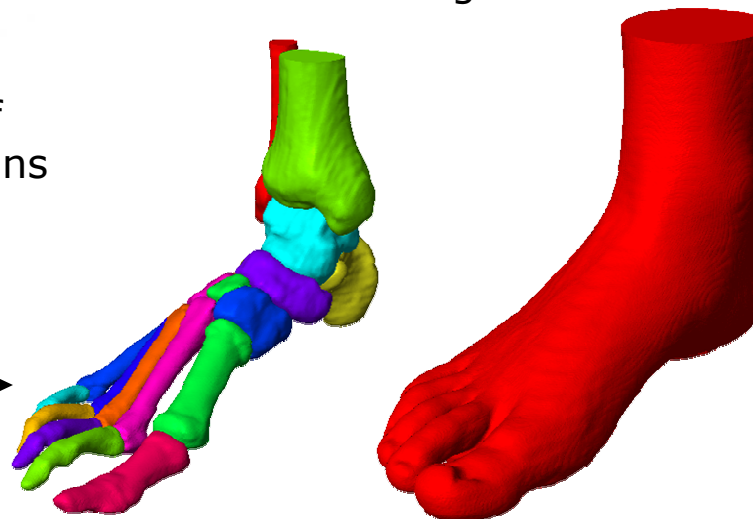
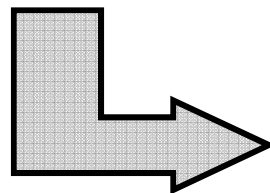
Toshiba® Aquilion 4  
(29 years old male)



345 slices  
1.00 mm slice distance  
512x512 image resolution



.STL format of  
segmented regions

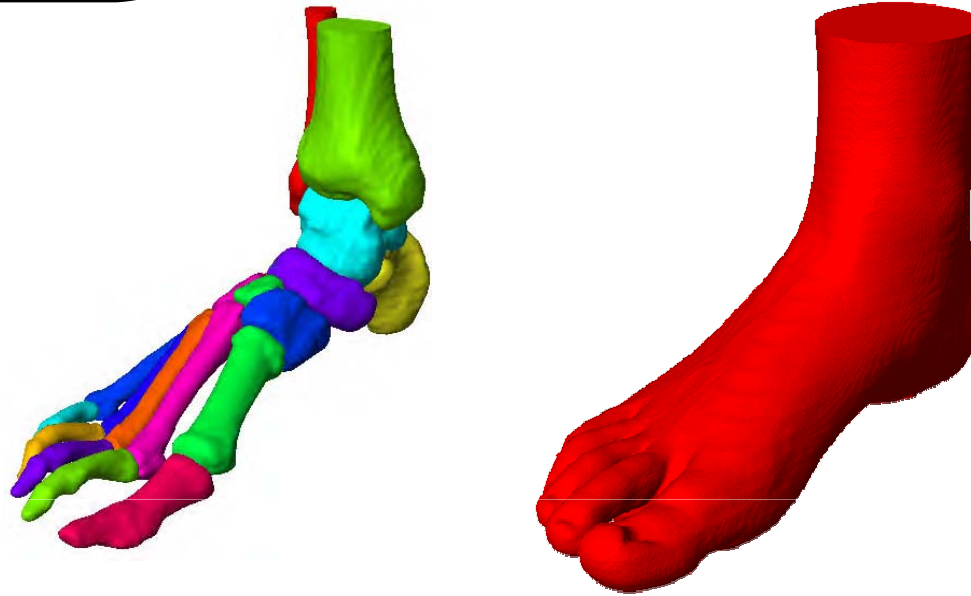


Bone structure and soft tissue

SCANIP® module, by  
Simpleware®, adopted

# Methodology Overview

## Image Processing



- ❑ 19 bones segmented: tibia, fibula, talus, calcaneus, cuboid, navicular, 3 cuneiforms, 5 metatarsals bones, 5 components of the phalanges
- ❑ Phalanges fused together since their relative motion do not affect plantar pressures
- ❑ Cartilages not extracted into the segmentation phase.

# Methodology Overview

Image Processing

**CAD Modeling**

- ❑ When Comsol Multiphysics® tries to directly import a tessellated model it generates some surface patches
- ❑ This procedure may generate some errors that user cannot directly control or fix
- ❑ Typically the geometry decomposition error is returned for imported multi-domain geometry
- ...
- ❑ ... then, CAD model was created into CAD system and so it was imported into Comsol Multiphysics®...



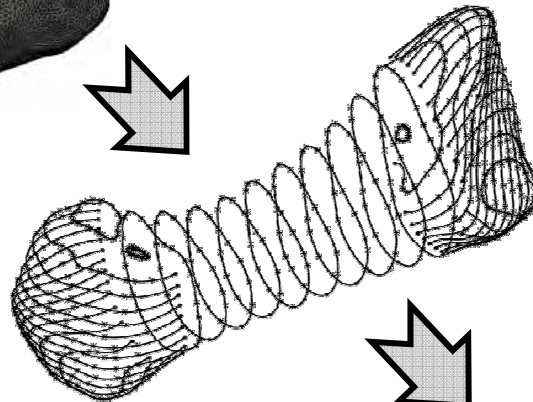
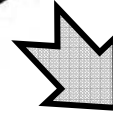
# Methodology Overview

Image Processing

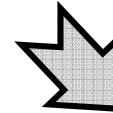
**CAD Modeling**



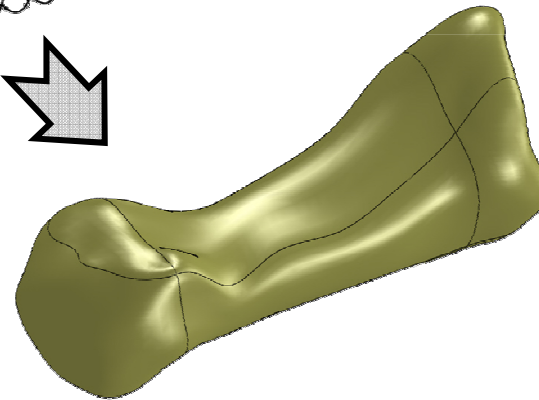
Tessellated model



Cross-section curves



3D CAD model



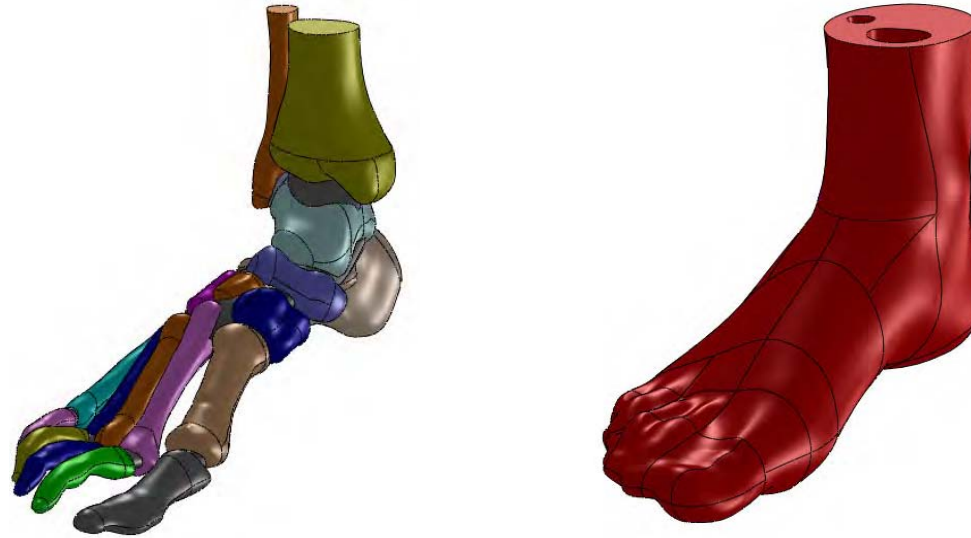
... starting from cross-sections  
lofting/sweeping/filling surfaces  
were generated...

SolidWorks® CAD system  
used with  
**SCANto3D®** add-in module

# Methodology Overview

Image Processing

CAD Modeling



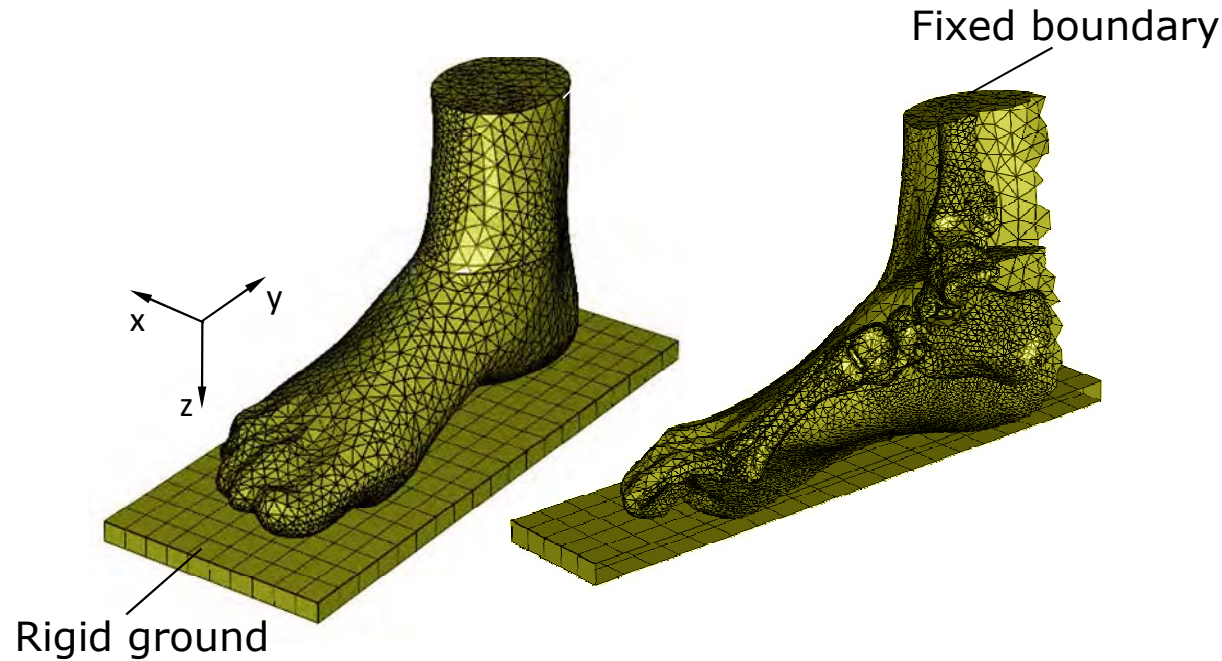
- ❑ Cartilages modeled in order to joint bones and fill the cartilaginous space
- ❑ Boolean operations used to ensure congruence among the related interfacial surfaces
- ❑ Toes at soft tissue level merged together.

# Methodology Overview

Image Processing

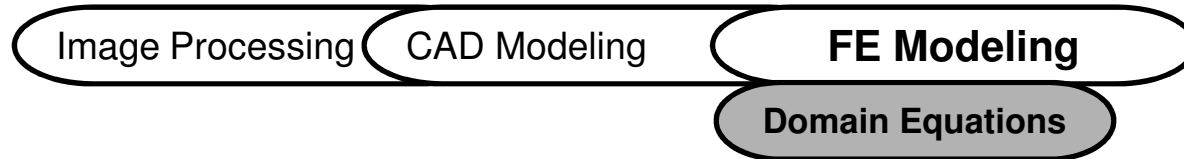
CAD Modeling

FE Modeling



- ❑ Domain equations, boundary conditions and solver settings provided
- ❑ The foot supposed to touch an ideal-rigid flat ground.

# Methodology Overview



- Soft tissue – **non-linear hyper-elastic behavior**

$$W(I I_1, I I_2, J) = C_{10} \cdot (I I_1 - 3) + C_{01} \cdot (I I_2 - 3) + C_{20} \cdot (I I_1 - 3)^2 + C_{11} \cdot (I I_1 - 3) \cdot (I I_2 - 3) + \dots$$

$$+ C_{02} \cdot (I I_2 - 3)^2 + \frac{1}{D_1} \cdot (J - 1)^2 + \frac{1}{D_2} \cdot (J - 1)^4$$

Constant	Value
$C_{10}$ (N/m <sup>2</sup> )	85550.0
$C_{01}$ (N/m <sup>2</sup> )	-58400.0
$C_{20}$ (N/m <sup>2</sup> )	38920.0
$C_{11}$ (N/m <sup>2</sup> )	-23100.0
$C_{02}$ (N/m <sup>2</sup> )	8484.0
$D_1$ (m <sup>2</sup> /N)	0.4370e-5
$D_2$ (m <sup>2</sup> /N)	0.6811e-6

- Bones – linear and isotropic material

$$E = 7300 \text{ MPa}, \nu = 0.3$$

- Cartilages – linear and isotropic material

$$E = 10 \text{ MPa}, \nu = 0.4$$

... data from literature

# Methodology Overview

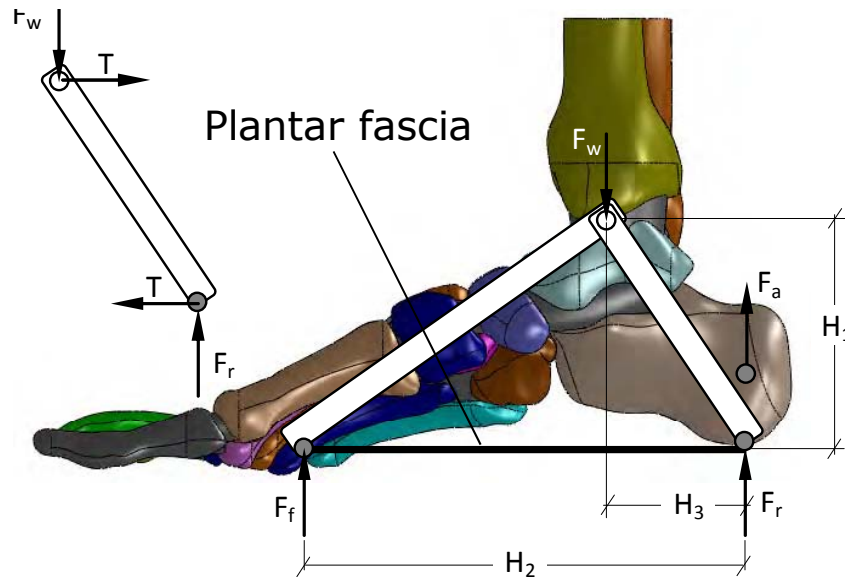
Image Processing

CAD Modeling

**FE Modeling**

Domain Equations

**Boundary Conditions**



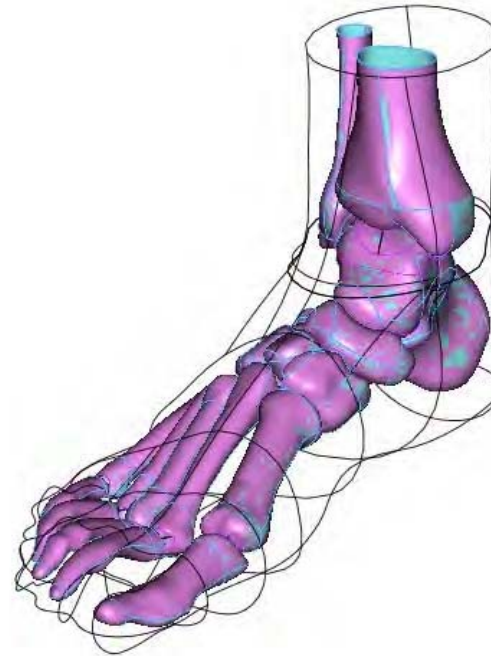
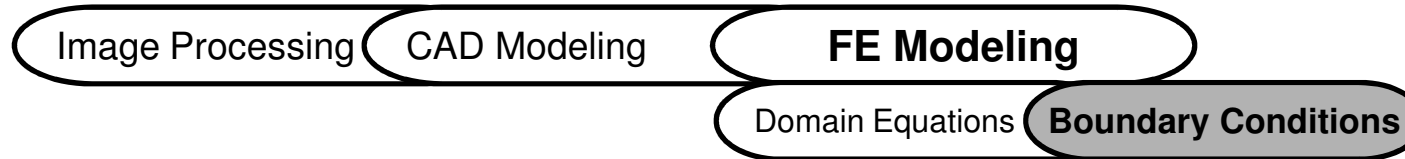
Equivalent Loads

$$\begin{cases} F_r = \frac{F_w \cdot (H_2 - H_3)}{H_2} \\ T \cdot H_1 = F_r \cdot H_3 \end{cases} \rightarrow T = \frac{F_w \cdot (H_2 - H_3)}{H_2} \cdot \frac{H_3}{H_1}$$

$$T = 0.4268 \cdot F_w$$

- ❑ A vertical force, corresponding to one half of the body weight ( $F_w=650/2$  N), transferred from the body to the foot and then to the ground
- ❑ The plantar fascia stabilizes the longitudinal arch of the foot and supports the longitudinal forces during the weight application phase
- ❑ Plantar fascia simplified and modeled by defining equivalent longitudinal forces ( $T \approx 0.5 \cdot F_w$ )

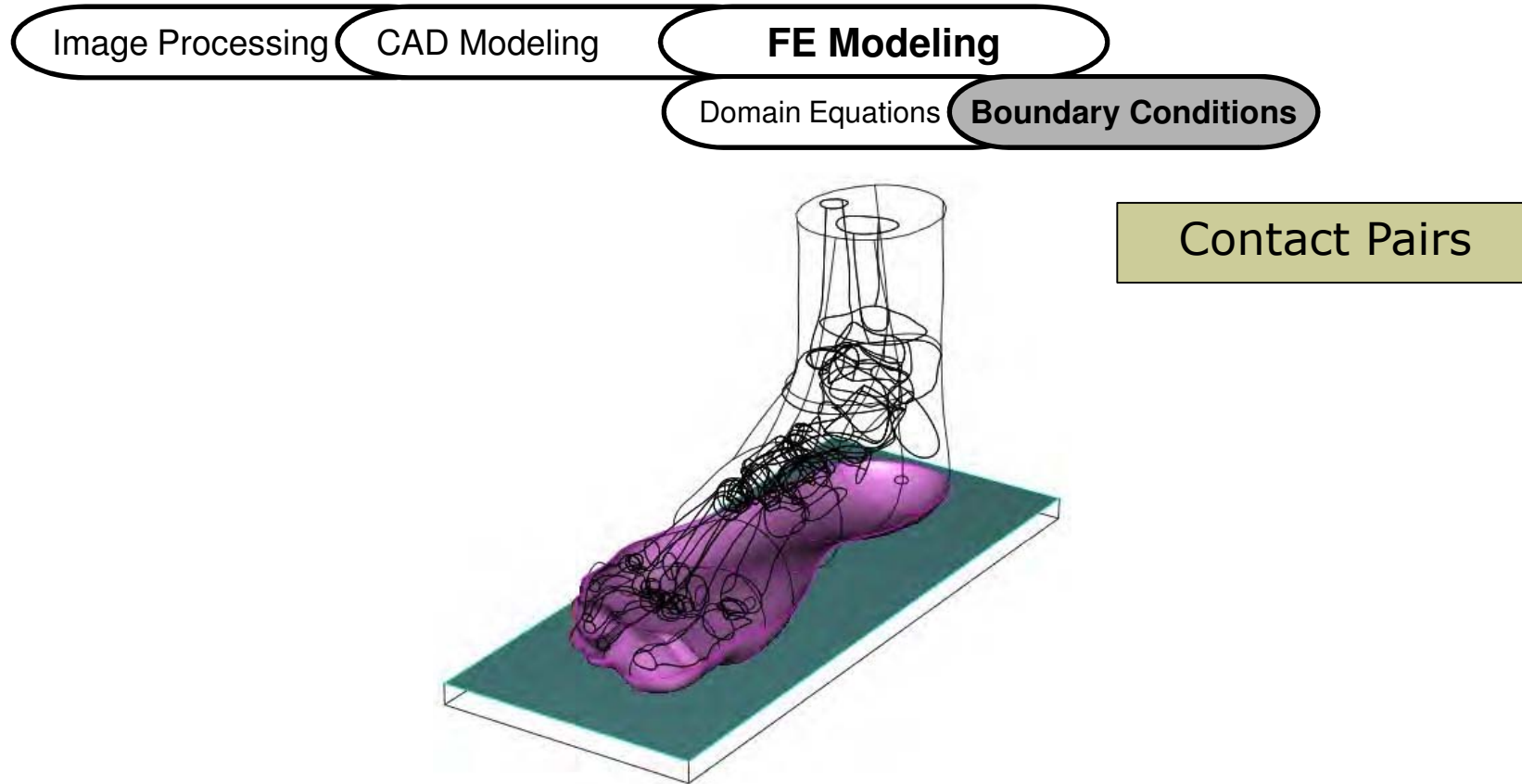
# Methodology Overview



Identity Pairs

- ❑ Physical interaction among bones-soft tissue and bones-cartilages modeled by defining identity pairs among interfacial surfaces.
- ❑ Displacement fields at interfacial surfaces are identical each-other.

# Methodology Overview



- Plantar pressures are of interest
- Contact pairs among plantar surfaces and ground-surface defined
- No friction accounted into the analysis
- Foot and ground supposed to be not in contact initially.

# Methodology Overview

Image Processing

CAD Modeling

FE Modeling

**Numerical Issues**

Contact Pairs

- Initial contact pressure:

$$P_n = 0 \text{ (no contact initially)}$$

- Scaling factor (related to contact pressure variables):

$$s_f = F_w / A_c \text{ (} F_w \text{: applied load. } A_c \text{: estimated final contact area)}$$

- Penalty factor:

$$p_n = s_c \cdot E_e / h_{\text{mesh}} \text{ (} s_c \text{: correction factor. } E_e \text{: equivalent elastic modulus.}$$

$h_{\text{mesh}}$ : mean mesh size)

... **Fine tuning** all these parameters was not a trivial task.

- ✓ With a “trial and error” approach, several experiments were conducted to carry out the optimal set of parameters, allowing to reach a valid solution into a reasonable time.



# Methodology Overview

Image Processing

CAD Modeling

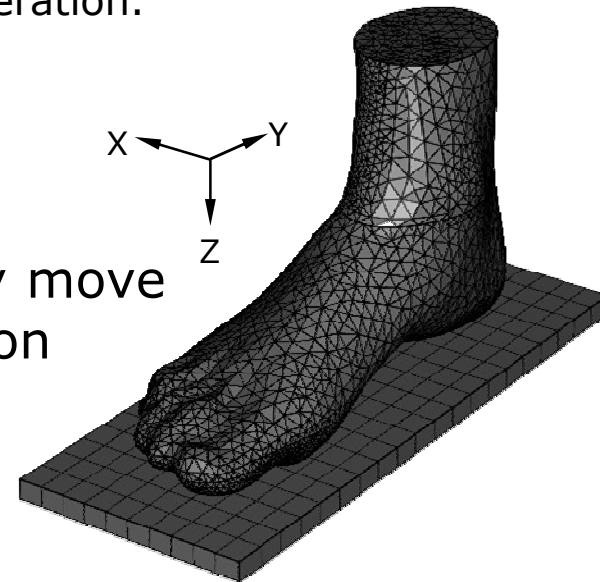
FE Modeling

**Numerical Issues**

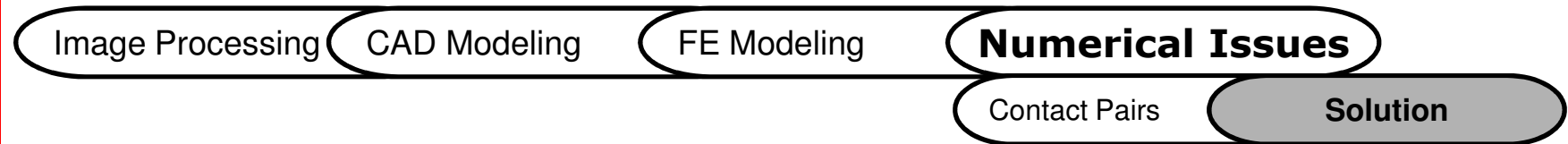
Contact Pairs

- ... Another feature to be considered, when managing and solving contact problems, is the **constraint status** of each domain
- ✓ "Lack of constraints" causes problems with the convergence process into Comsol Multiphysics®
  - ✓ All domains should be constrained in all directions, so that there is only one possible solution for each convergence iteration.

Ground domain supposed to rigidly move only along the global Z direction



# Methodology Overview

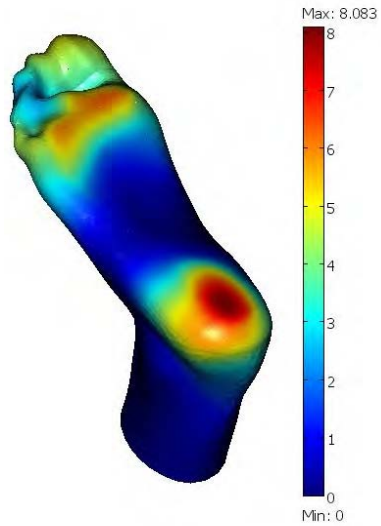


- Parametric solver adopted
- “PARDISO out of core” adopted as linear solver
- Final mesh made of 25812 nodes and 87149 elements
- Linear shape function used
- # of DoF solved for equal to 81428

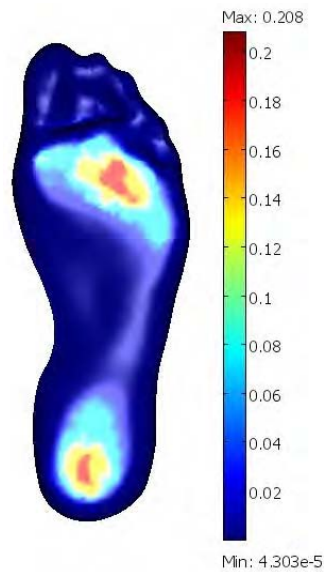
Numerical simulations were accomplished in about **100 min**

DELL Precision T7400 workstation  
(WinXP 64bit, 16GB RAM, 2 Xeon E5420 quad-core processors)

# Result Analysis



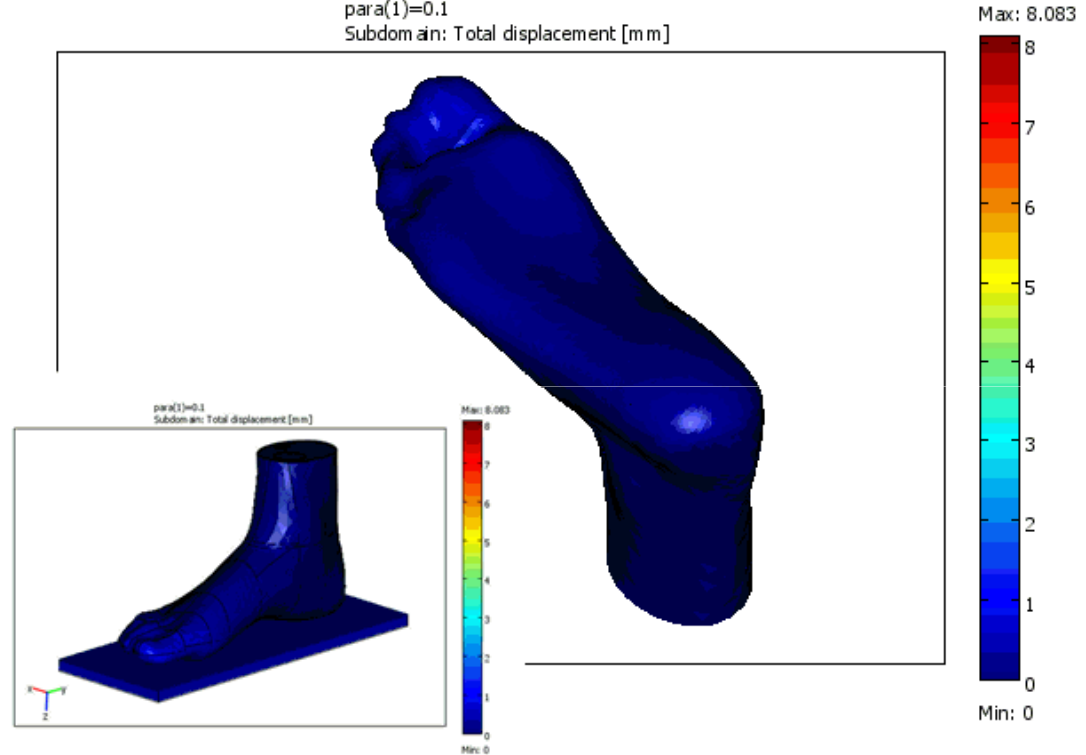
Total displacement [mm]



Plantar pressure map [MPa]

## Movie-total displacement

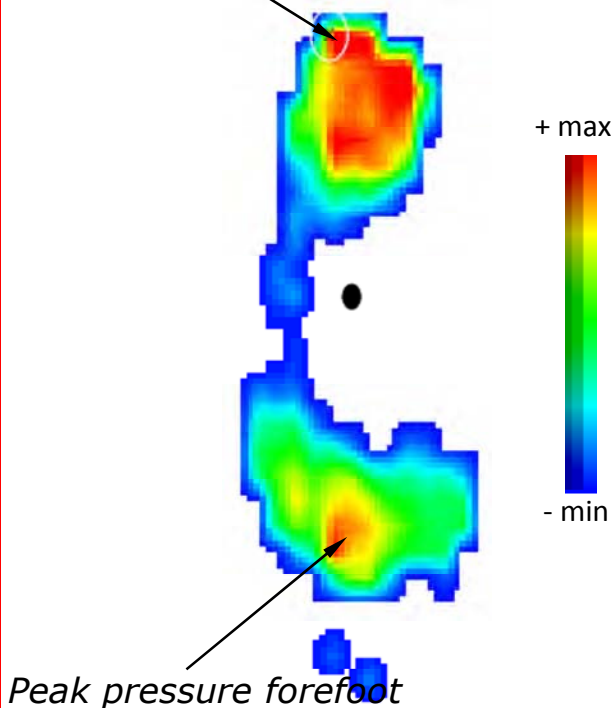
para(1)=0.1  
Subdomain: Total displacement [mm]



# Experimental Validation

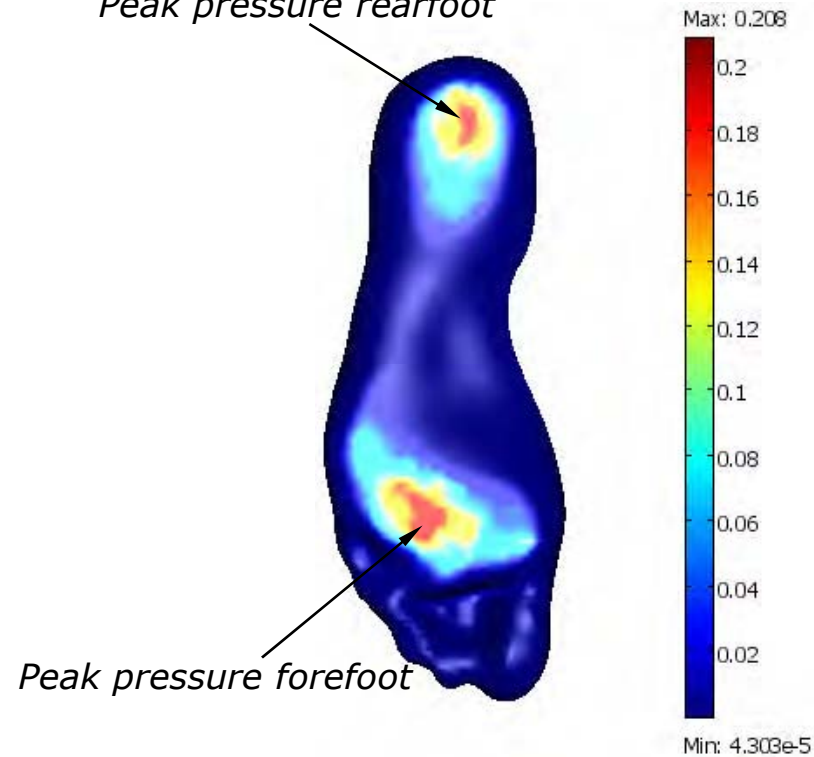
... high resolution insole sensors used to validate numerical results

*Peak pressure rearfoot*



Experimental results

*Peak pressure rearfoot*



Numerical results [MPa]

**... regions with the peak pressure can be compared**

# Final Remarks

- ❑ Simulation of the balanced standing condition of a human foot model:
  - ✓ CAD model created from CT images
  - ✓ Hyper-elastic non-linear material law set
  - ✓ Contact pairs introduced to calculate plantar pressure maps
- ❑ Numerical issues pointed out:
  - ✓ Best choice of convergence parameters comes from some general rules along with a trial-and-error approach.
  - ✓ Manual fine-tuning numerical parameters is a very time consuming task.

**... so, some improvements and suggested best practices to resolve model involving contact pairs are expected in the next future**



**Thanks for your attention!**

**Questions?**

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