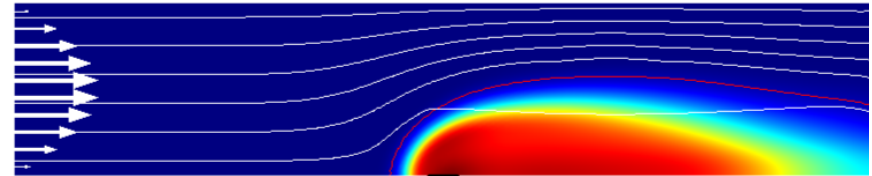


Effects of flow and diffusion on blood coagulation in platelet poor plasma

A two-way coupling between hemodynamics and biochemistry

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Bart Bakker, Rene van den Ham,
Luca Formaggia



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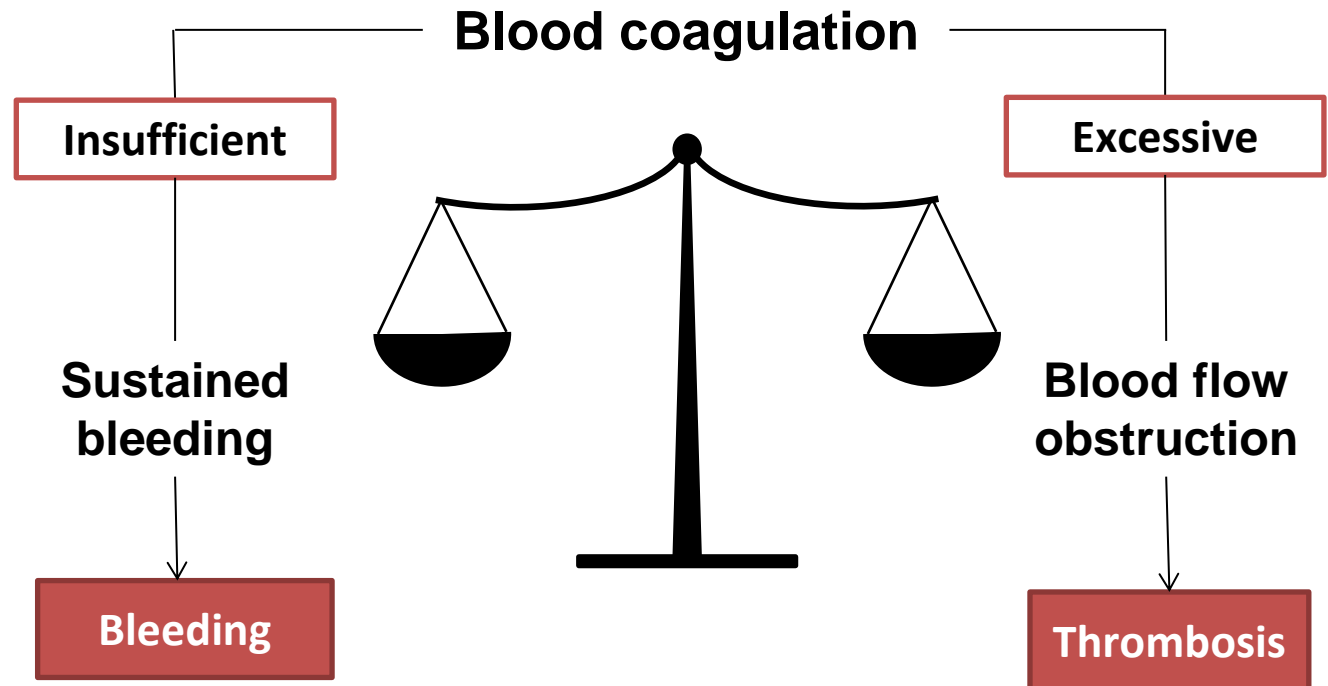


POLITECNICO DI MILANO
Mathematical Department
«F. Brioschi»

Blood coagulation

Outline and motivation

- Biological background
- Mathematical and numerical model
- Results and analysis
- Conclusions



Biological background

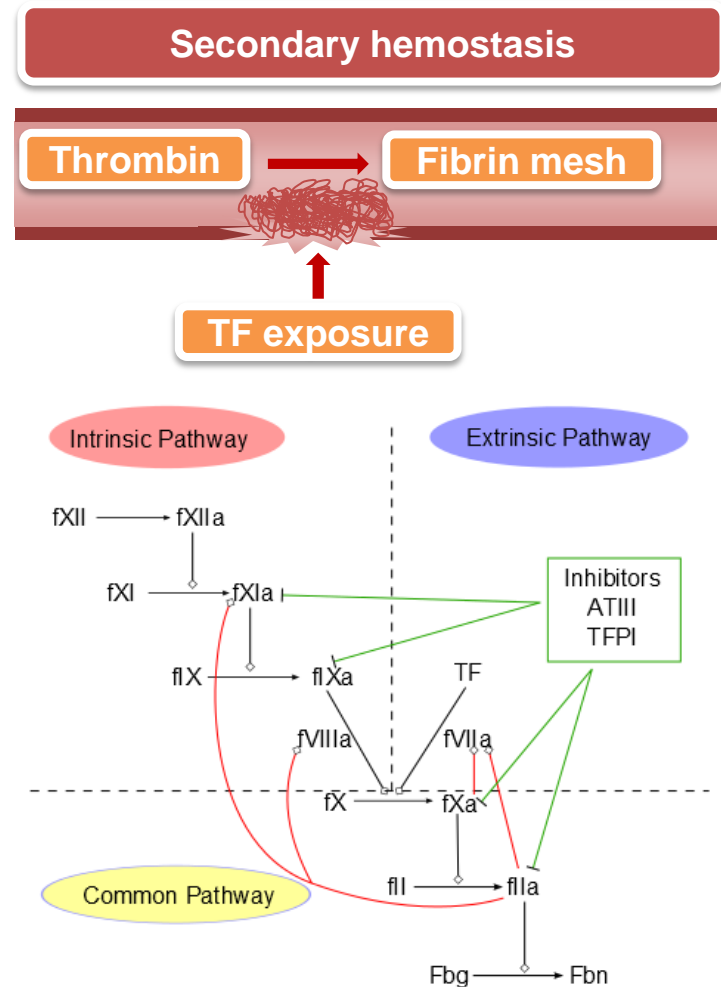
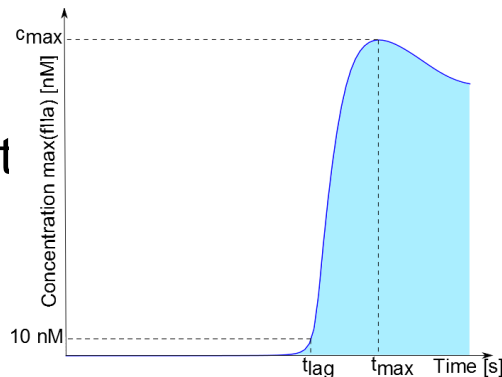
Secondary hemostasis in platelet poor plasma

Coagulation network

- Tissue factor: TF
- Inhibitors
- Feedback loops
- Thrombin: fIIa
- Fibrin: Fbn

Output parameters

- Thrombogram: t_{lag} , t_{max} , C_{max}
- TGD
- t_{clot} , A_{clot}
- Wound-Clot



Mathematical and numerical method

Coagulation network

Plasma species in Ω , $t > 0$

$$\frac{\partial \mathbf{c}_p(\mathbf{x}, t)}{\partial t} - D \nabla^2 \mathbf{c}_p(\mathbf{x}, t) + \mathbf{u}(\mathbf{x}, t) \cdot \nabla \mathbf{c}_p(\mathbf{x}, t) = R_p(\mathbf{c}(\mathbf{x}, t))$$

Membrane species on Γ_{down} , $t > 0$

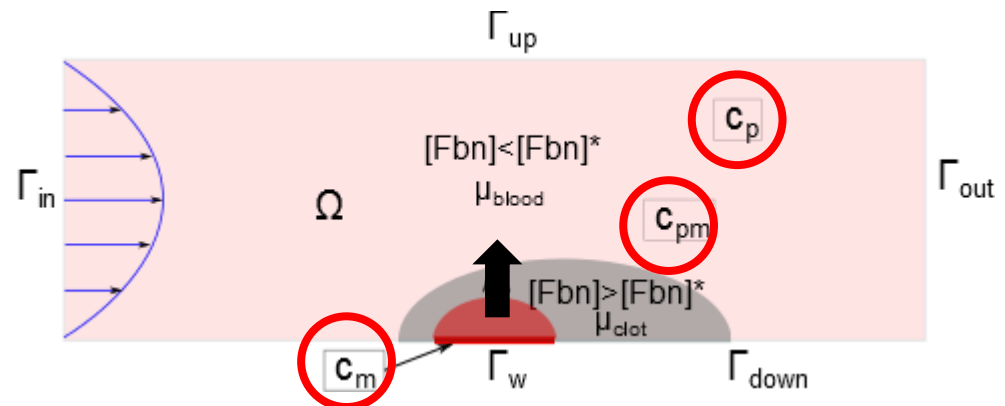
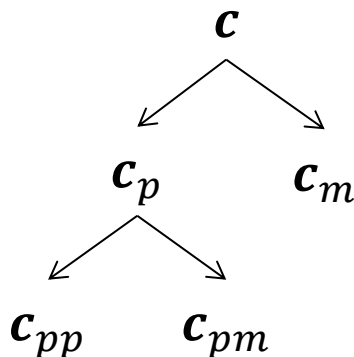
$$\frac{\partial \mathbf{c}_m(\mathbf{x}, t)}{\partial t} = R_m(\mathbf{c}(\mathbf{x}, t))$$

Coupling by boundary conditions on Γ_{down} , $t > 0$

$$-\mathbf{n} \cdot D \nabla \mathbf{c}_{pm}(\mathbf{x}, t) = R_{pm}(\mathbf{c}(\mathbf{x}, t))$$

46 PDEs
11 ODEs (Γ_{down})
1 ODE (Ω)
58 equations

Linear finite elements
method with streamline and
crosswind numerical
diffusion



Mathematical and numerical method

Blood flow

Modified **Navier-Stokes** equations in Ω , $t > 0$

$$\rho \frac{\partial \mathbf{u}}{\partial t} + \rho \mathbf{u} \cdot \nabla \mathbf{u} = \nabla \cdot [-p\mathbf{I} + \mu(\mathbf{x}, t)(\nabla \mathbf{u} + \nabla^T \mathbf{u})]$$

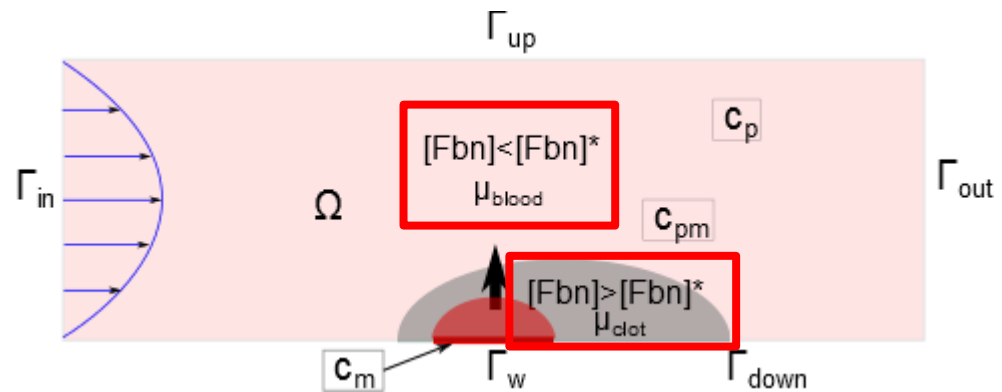
$$\nabla \cdot \mathbf{u} = 0$$

Viscosity depending on fibrin (threshold $[\text{Fbn}]^*$)

$$\mu(\mathbf{x}, t) = \mu([\text{Fbn}]) = \begin{cases} \mu_{\text{blood}} & \text{if } [\text{Fbn}] < [\text{Fbn}]^* \\ \mu_{\text{clot}} & \text{if } [\text{Fbn}] \geq [\text{Fbn}]^* \end{cases}$$

Laminar flow

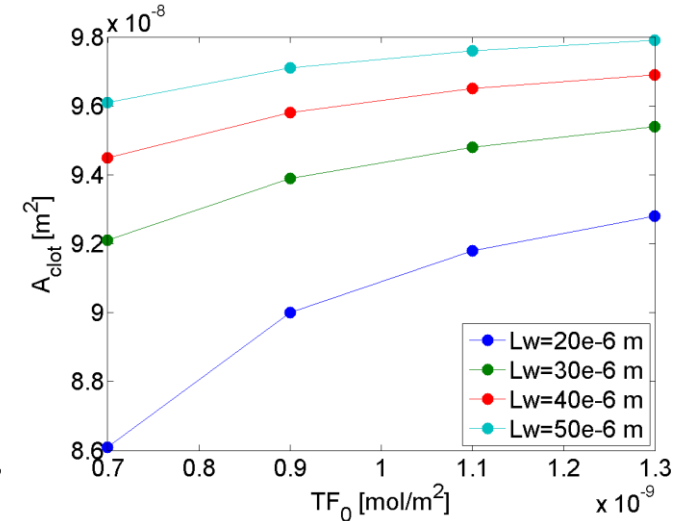
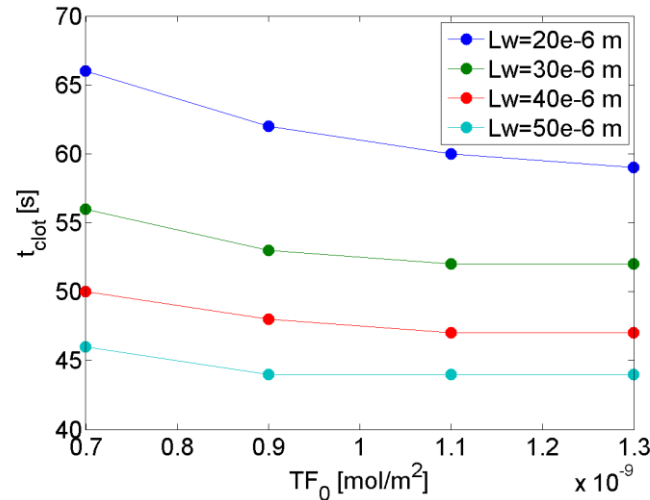
P_1P_1 with
streamline and
crosswind
diffusion



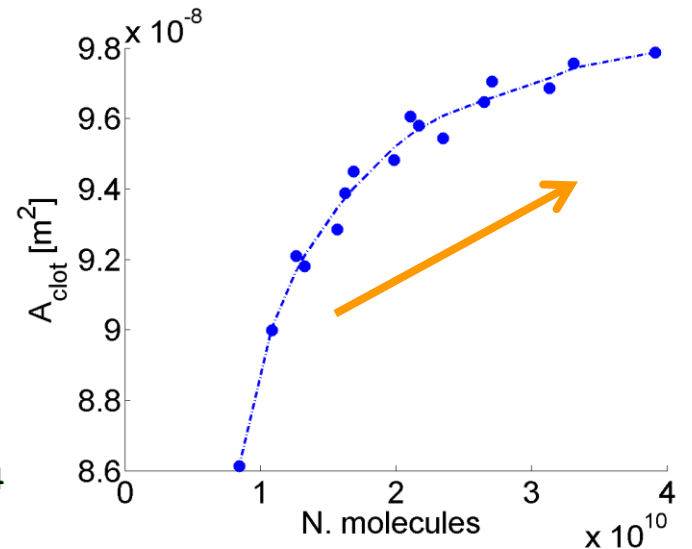
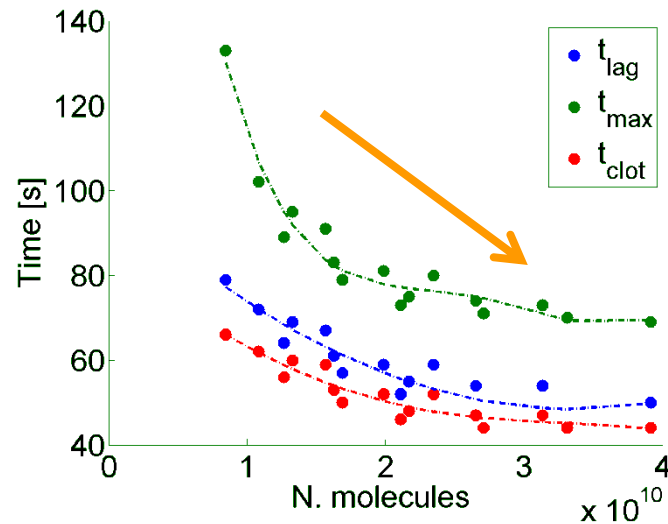
Results

Tissue factor and wound size

TF_0 [fmol/cm ²]	L_w [μ m]
70	20
90	30
110	40
130	50



TF_0 or $L_w \uparrow$	
t_{max}	\downarrow
t_{lag}	\downarrow
t_{clot}	\downarrow
C_{max}	\uparrow
A_{clot}	\uparrow
TGD	\uparrow

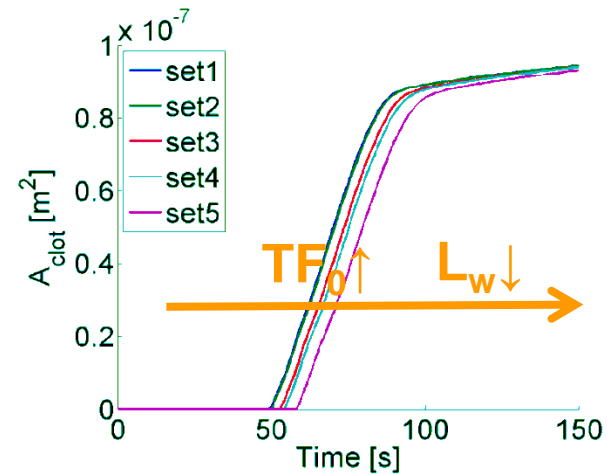
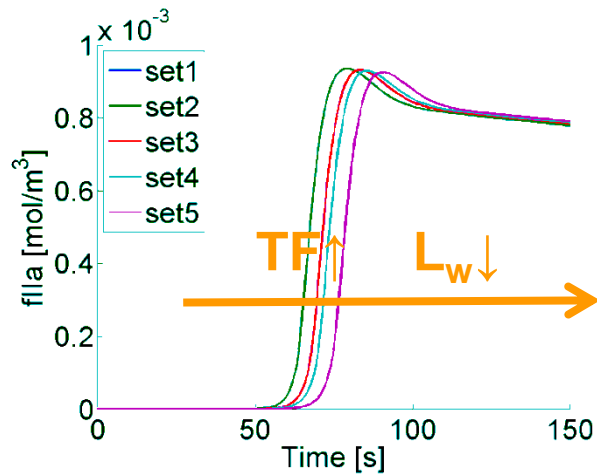


Results

Constant number of molecules

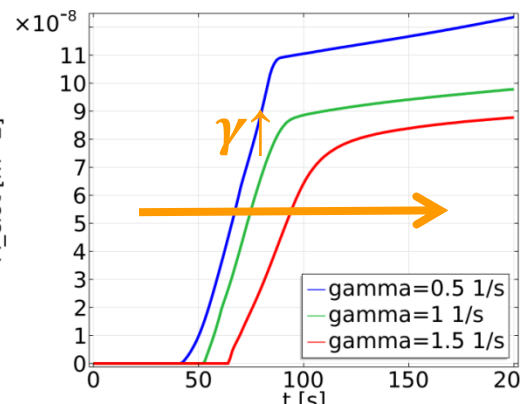
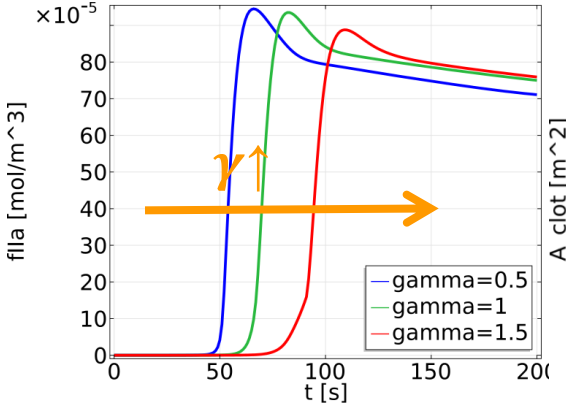
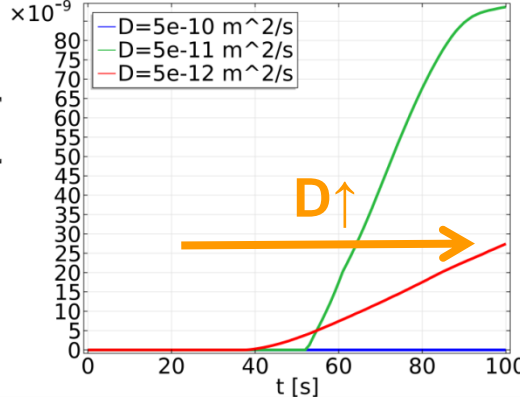
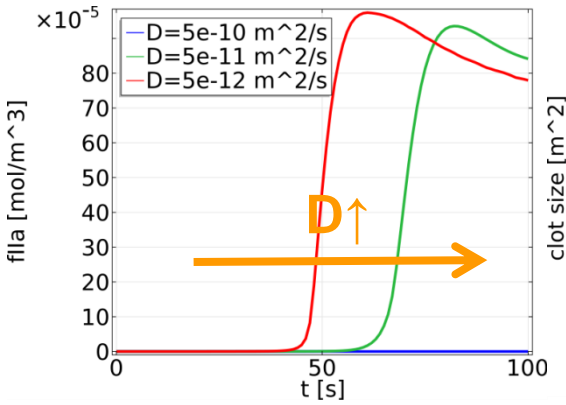
Set	TF_0 [fmol/cm ²]	L_w [μ m]
1	67.5	40
2	70	38.6
3	90	30
4	110	24.5
5	135	20

- Spatial distribution dominates over concentration level
- Contact region
- Contact time



Results

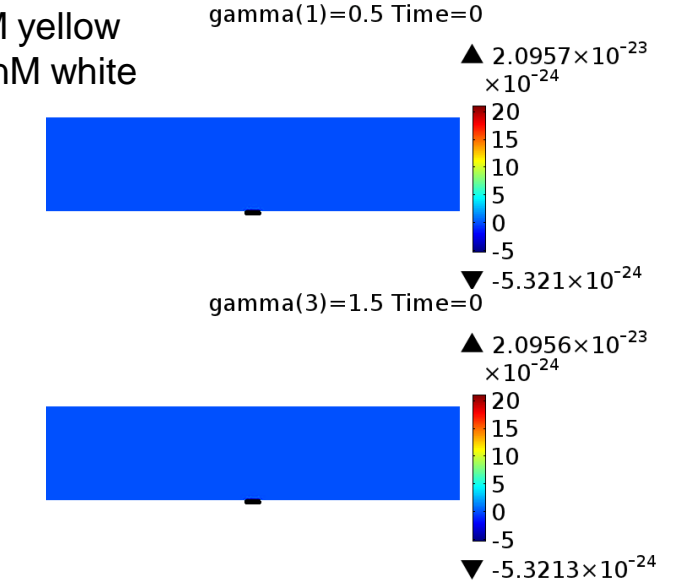
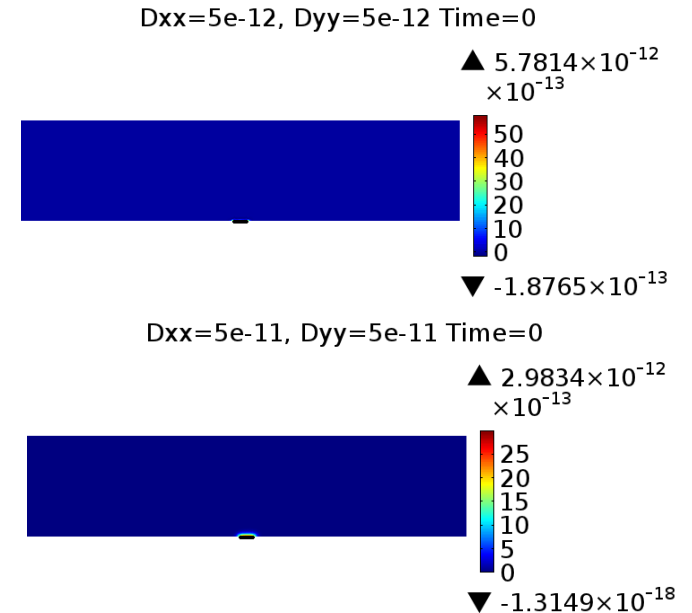
Flow and diffusion



- Contour level
- flla=10nM yellow
 - Fbn=600nM white

DIFFUSION

FLOW



Conclusions

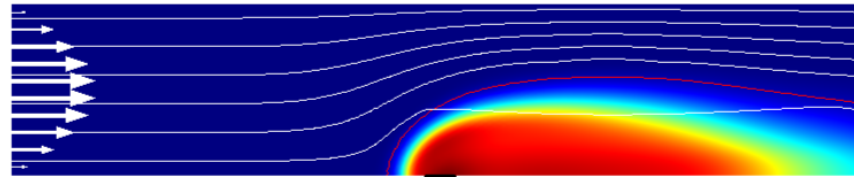
- Increasing TF_0 or L_w enhances blood coagulation
 - stronger and accelerated burst
 - Larger clot and earlier clot occurrence
- Coagulation response is more sensitive to variation in L_w than TF_0
 - Contact region/time
- Flow and diffusion have a limiting role on blood coagulation
 - Delayed and damped burst
 - Domination of the anticoagulant effect

PRO-COAGULANT
EFFECT

ANTI-COAGULANT
EFFECT

Thank you for your attention

Questions



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