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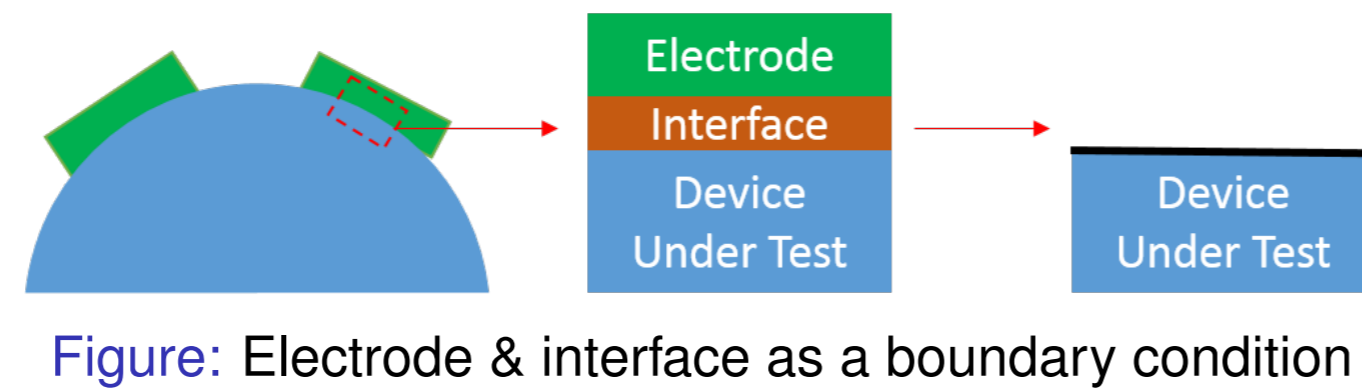
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Introduction: electrical imaging

Metallic electrodes for current injection & potential measurements
How to take into account contact impedances ?

Complete Electrode Model [1] in Electrical Impedance Tomography [2]

$$\begin{cases} -\nabla \cdot (\sigma \nabla v) = 0 & \forall x \in \Omega \\ v + z_e \sigma \nabla v \cdot \mathbf{n} = v_e & \forall x \in E_e \\ \int_{E_e} \sigma \nabla v \cdot \mathbf{n} d\Gamma = i_e & \forall e = 1 \dots E \\ \sigma \nabla v \cdot \mathbf{n} = 0 & \forall x \in \partial\Omega \setminus \bigcup_{e=1}^E E_e \end{cases}$$



Literature solutions

1. Custom-built finite element method (FEM) -based libraries, e.g. EIDORS [3]
Development & debugging costs, simplistic computation assumptions, augmented stiffness matrix
2. Model the thickness of electrodes within generalist FEM packages, e.g. COMSOL [4]
Huge number of uninformative degrees of freedom, how to recover sensitivity patterns ? [5]

Methods

Data predictions

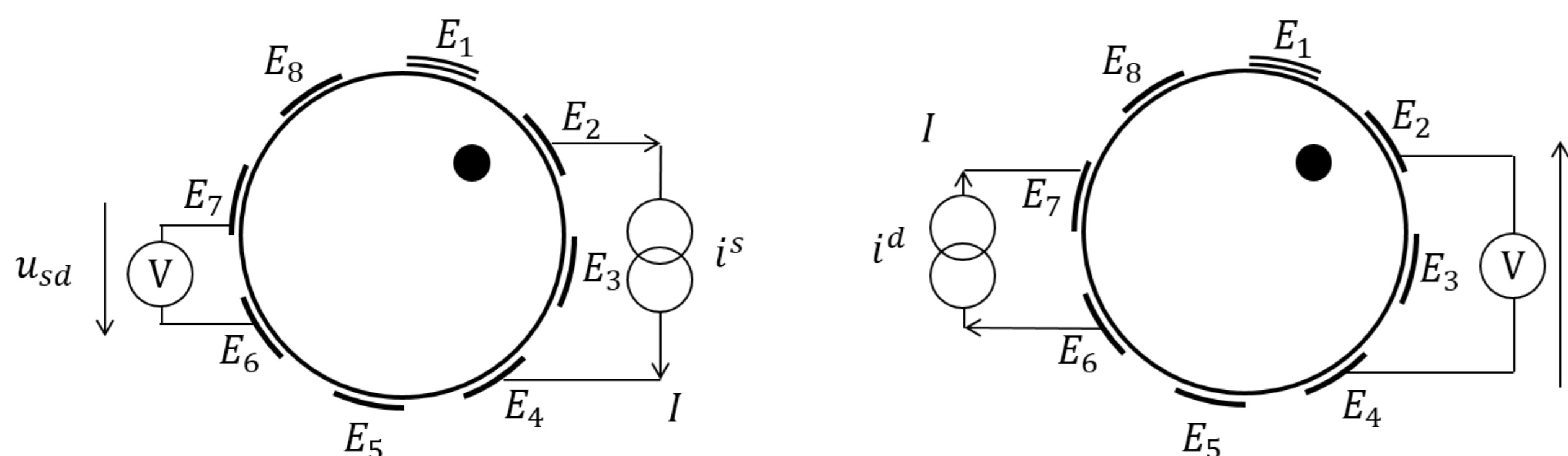
Single NEUMANN boundary condition

Couple both current injection & contact impedance on a boundary

$$-\mathbf{n} \cdot \mathbf{j} = \frac{1}{z_e \|E_e\|} \left(\int_{E_e} v d\Gamma + z_e i_e - \|E_e\| v \right)$$

Electrode potentials deduced during post-processing

Sensitivity analysis



$$\frac{\partial u_{sd}}{\partial \sigma_c} = \frac{-1}{I} \int_{\Omega_c} \nabla v(i^s) \cdot \nabla v(i^d) d\Omega$$

VORONOÏ cells as control volumes [7]

Nodal approximation of electric fields

$$[\mathbf{J}]_{sd,n} = \frac{\partial u_{sd}}{\partial \sigma_n} = \frac{-\|\Pi_n\|}{I} \nabla v_n(i^s) \cdot \nabla v_n(i^d)$$

Parameter estimation : absolute or differential

Inverse problem operation

1. Comsol optimization module [8]

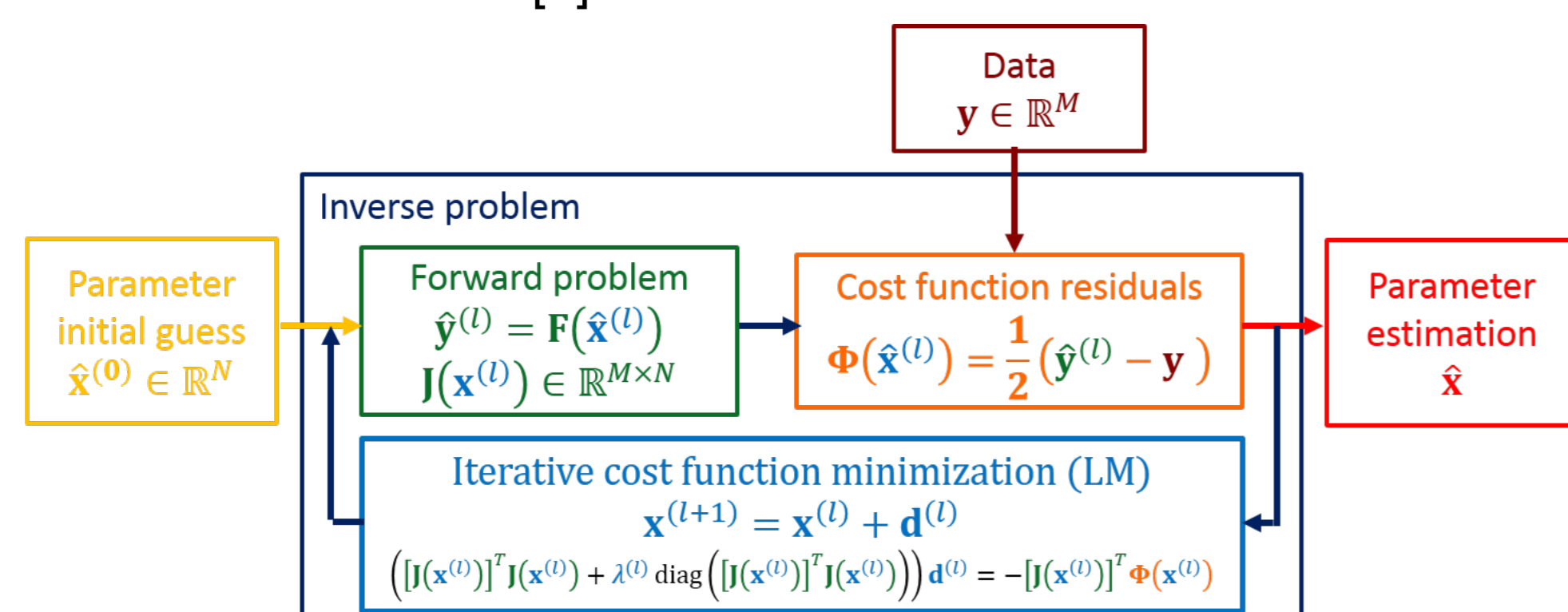


Figure: Absolute inversion in EIT using COMSOL : forward problem & cost function residuals are handled by a first component ; the optimization is operated by a second component, e.g. through a LEVENBERG - MARQUARDT algorithm

2. Any EIT inversion algorithm [2,9]
can rely on the proposed forward solver to reconstruct conductivity maps

Results

Forward solver

Verified versus analytic solutions, Test cases in 2D & 3D (1 mA, 1 S · m⁻¹)

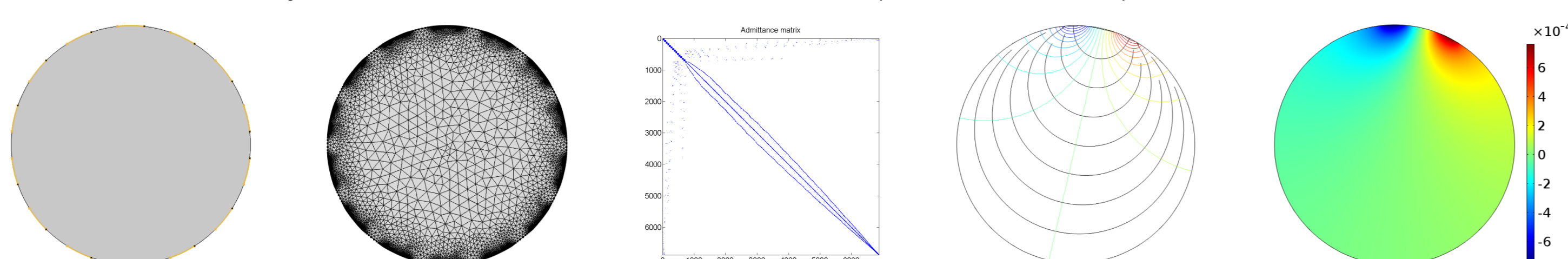
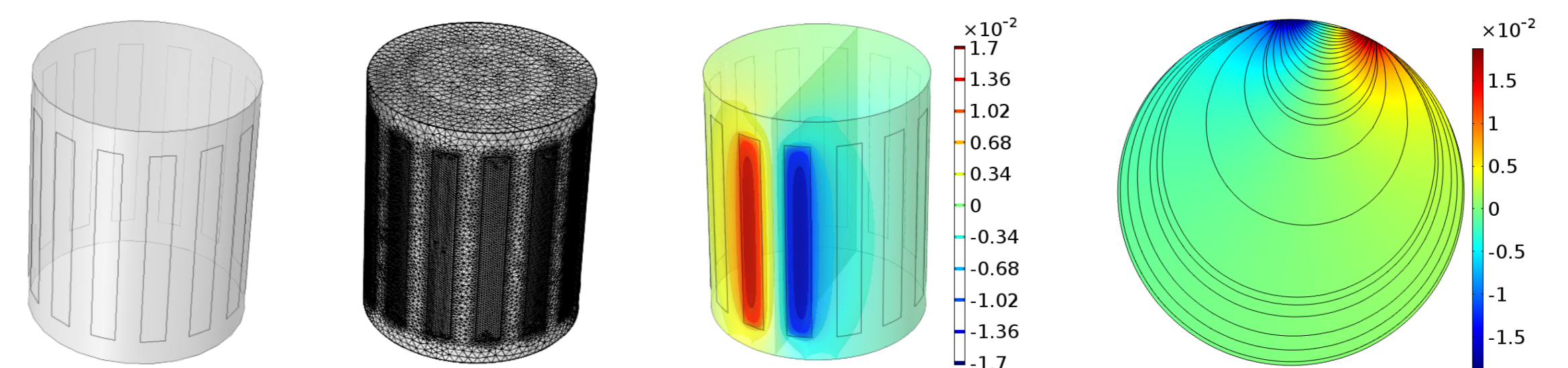
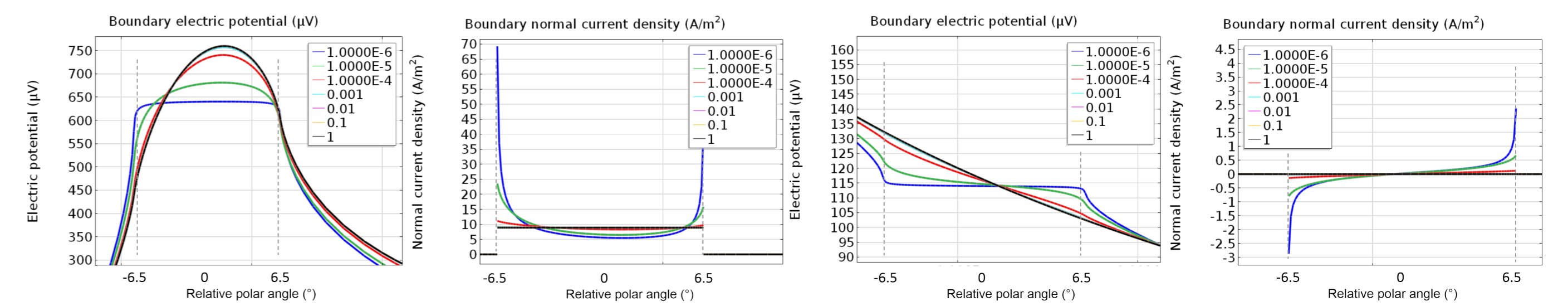
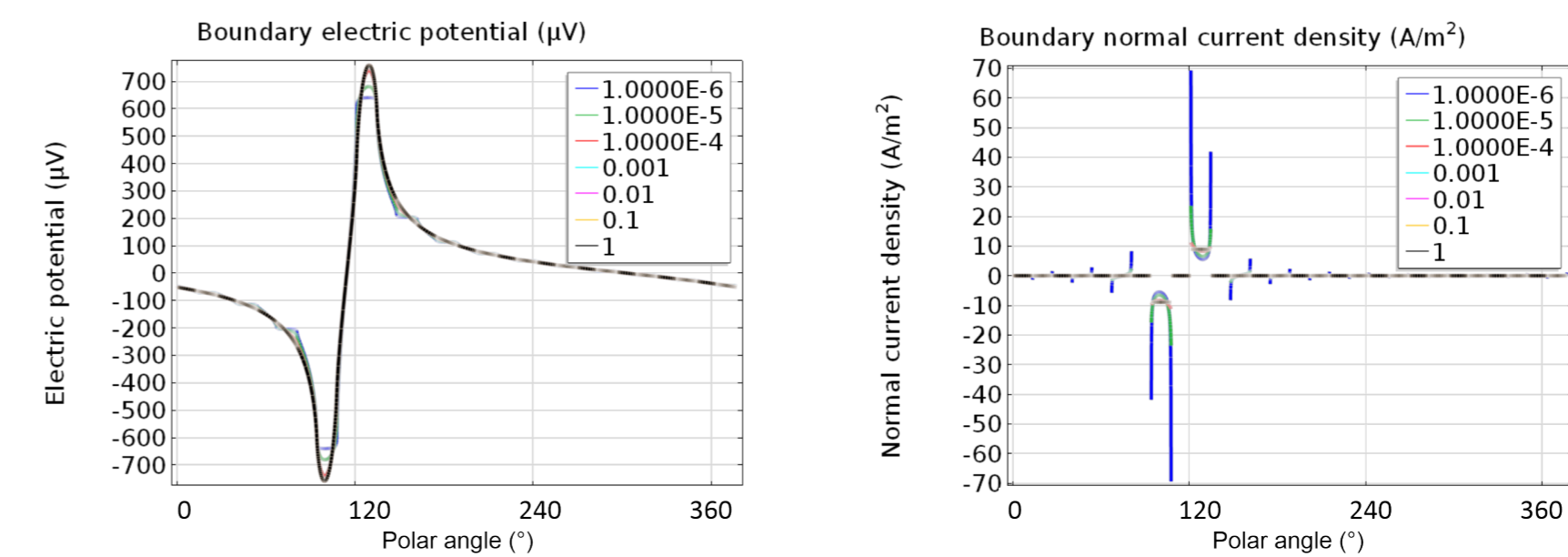


Figure: 2D test case: electrodes as boundaries, corresponding mesh, associated stiffness matrix, equipotentials and current density streamlines for the first projection

Influence of electrodes on the potential distribution, edge effects due to contact impedances



Benchmarking: EIDORS versus COMSOL

Figure of merit (FoM): maximum of relative error

Test case	FoM Node potentials	FoM Electrode potentials	CPU time (EIDORS / COMSOL) *
2D	10 ⁻¹⁰	10 ⁻¹²	26 s / 10 s
3D	10 ⁻⁴	10 ⁻⁷	330 s / 550 s

* CPU time encompasses only assembly of the stiffness matrix and solving in EIDORS while it also includes meshing in COMSOL

Reconstructions

Absolute inverse conductivity problem

Discontinuous GALERKIN elements (inverse mesh) within COMSOL optimization module

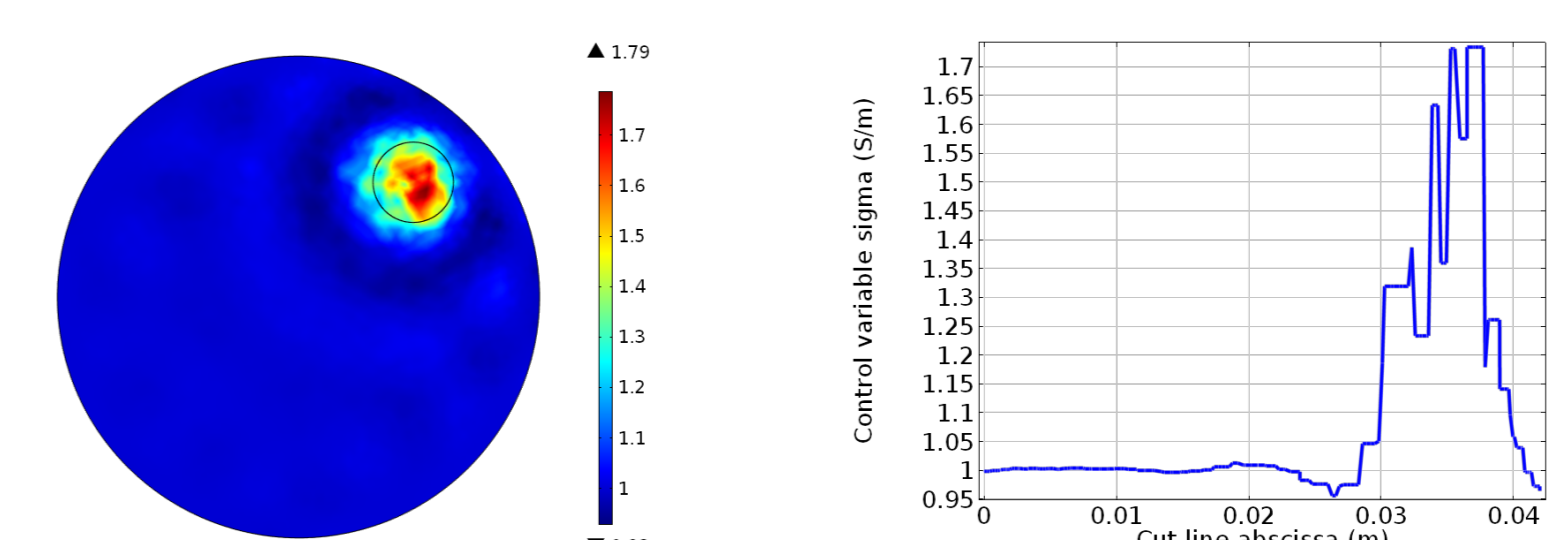


Figure: 2D absolute reconstruction on synthetic data: estimated conductivity map & profile along first diagonal

Differential inverse conductivity problem

Simplices for sensitivity computations inside COMSOL, parameter estimation in Matlab [9]

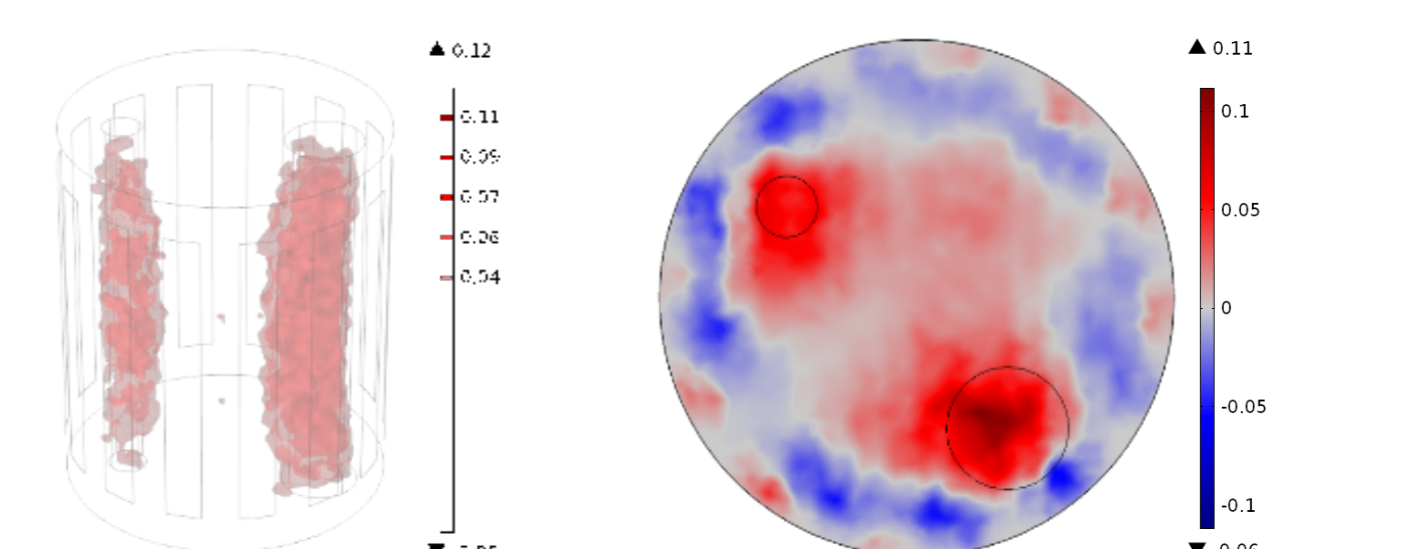


Figure: 3D differential reconstructions on *in vitro* data [10]: thresholded isosurfaces & cross-sectional map of estimated conductivity variation

Discussion et Perspectives

Versatile forward solver

- Consistent numerical approximation with previous developments
- Complete framework for EIT, with inverse problem capabilities
- Extensions to other electromagnetic situations
e.g. tDCS, EEG, DBS (forward & inverse problems)

Future developments towards

- Incorporation of advanced regularization strategies
- Adaptive forward / inverse meshing schemes
- Multispectral capabilities
- Reducing CPU time for inverse problems & 3D models

References

- [1] Somersalo et al., "Existence and Uniqueness for Electrode Models for EIT", *SIAM J. Appl. Math.* 52(4), 1992
- [2] Seo et al., "Electrical Impedance Tomography", in *Nonlinear Inverse Problems in Imaging*, Wiley, 2013
- [3] Adler et al., "Uses and abuses of EIDORS: an extensible software base for EIT", *Physiol. Meas.* 27(5), 2006
- [4] Pettersen et al., "From 3D tissue data to impedance using Simpleware ScanFE+IP and COMSOL", *J.E.B.* 2 (1), 2011
- [5] Lionheart, "EIT reconstruction algorithms: pitfalls, challenges and recent developments", *Physiol. Meas.* 25 (1), 2004
- [6] Geselowitz, "An Application of ECG Lead Theory to Impedance Plethysmography", *IEEE TBME* 18(1), 1971
- [7] Fouchard et al., "Méthodes numériques pour le problème direct et l'analyse de sensibilité en EIT", GRETSI, 2015
- [8] Cardiff et al., "Efficient solution of nonlinear, underdetermined inverse problems", *Comp. Geosciences* 34(11), 2008
- [9] Fouchard et al., "Inversion without effective jacobian calculations in EIT", *J. Physics: conf. series*, 2014
- [10] Fouchard et al., *Modular architecture of a MfEIT system*, IEEE EMC, 2014