

Analysis of PhotoThermal Ablation

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Outline

- Motivation
- Implementation
- Verification
- Application



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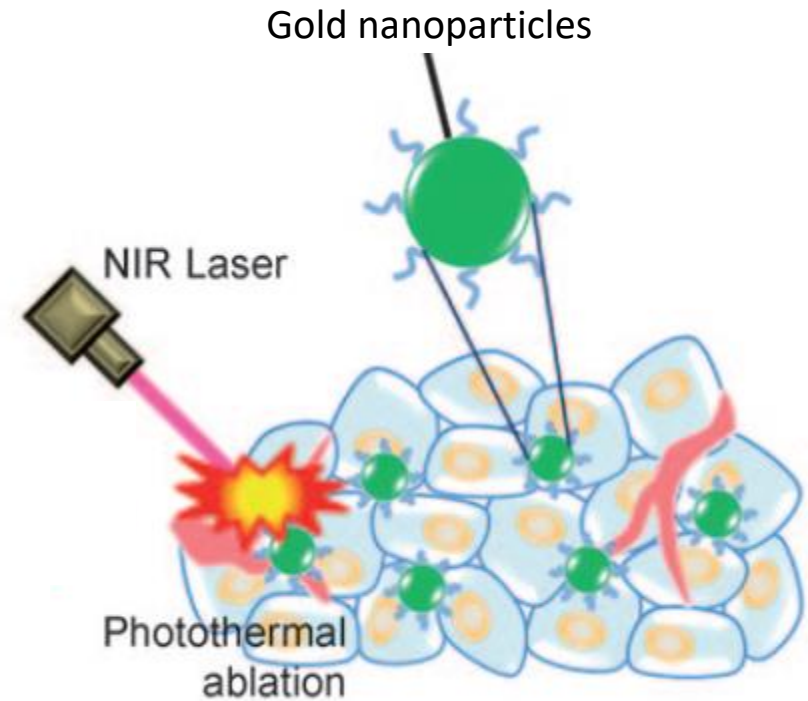
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Tumor ablation

- Cancer tumors
- Tissue necrosis
 - Cancer cells irreversibly damaged at 42°C
 - Normal cells can survive up to 47°C
- Tumors have limited vascularity
 - Inability to disperse heat
- Minimally invasive ablation
 - Radiofrequency
 - Microwave
 - Laser

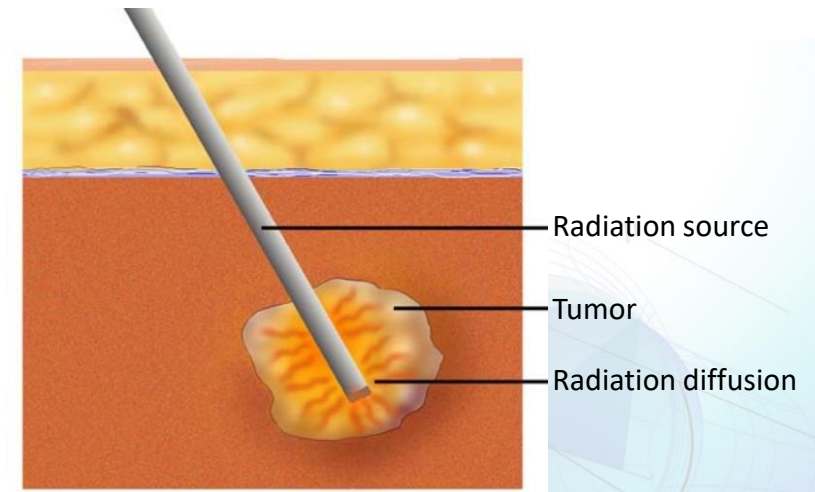
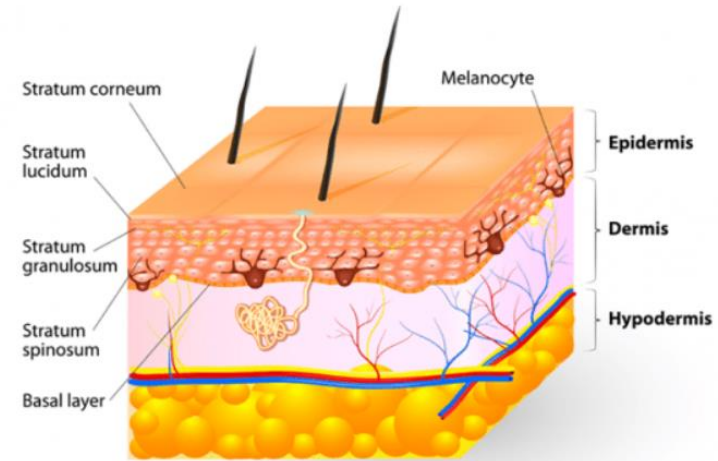
PhotoThermal Ablation

- Improved localization of treatment
- Laser interaction with photothermal sensitizers
- Gold nanoparticles
- Near IR laser radiation for tissue penetration
- Localized generation of heat



COMSOL Multiphysics® model

- Light diffusion in tissue
 - Irradiance distribution
- Layered tissue structure
- Heat transfer due to absorption of light
- Heat dissipation
 - Perfusion
 - Convection from outer surface



Governing equations

- Time dependent diffusion:

$$\frac{1}{c} \frac{\partial}{\partial t} \Phi + \nabla \cdot -(D \nabla \Phi) = -\mu_a \Phi + S$$

Φ : photon fluence (number of photons per unit area per unit time), $[1/(m^2 \cdot s)]$
 $D = 1/[3(\mu_a + \mu'_s)]$: optical diffusion coefficient, $[m]$
 μ_a : absorption coefficient $[1/m]$
 μ'_s : reduced scattering coefficient, $[1/m]$
 c : speed of light in tissue, $[m/s]$
 S : source, other than that due to absorption $[1/(m^3 \cdot s)]$

- Fluence flux:

$$\Gamma = -D \nabla \Phi,$$

COMSOL Multiphysics® implementation

- General form PDE interface
- Tissue properties defined in the Parameters node

$$\frac{1}{c} \frac{\partial}{\partial t} \Phi + \nabla \cdot \underbrace{(-D \nabla \Phi)}_{\text{Flux } \Gamma} = \underbrace{-\mu_a \Phi}_{\text{Sink term}} + S$$

\uparrow
 d_a

Label: General Form PDE 1

Equation: Study 1, Time Dependent

$\epsilon_a \frac{\partial^2 u}{\partial t^2} + d_a \frac{\partial u}{\partial t} + \nabla \cdot \Gamma = f$ ← Eq. (1)

Conservative Flux

Γ	$-ux*D$	x	1/(m ² ·s) ← Flux, Eq. (2)
	$-uy*D$	y	
	$-uz*D$	z	

Note: $\{ux, uy, uz\} = \left\{ \frac{\partial}{\partial x}, \frac{\partial}{\partial y}, \frac{\partial}{\partial z} \right\}$

Source Term

f $-mua*u$ 1/(m³·s) ← Sink term in Eq. (1)

Damping or Mass Coefficient

d_a $1/c$ s/m

Mass Coefficient

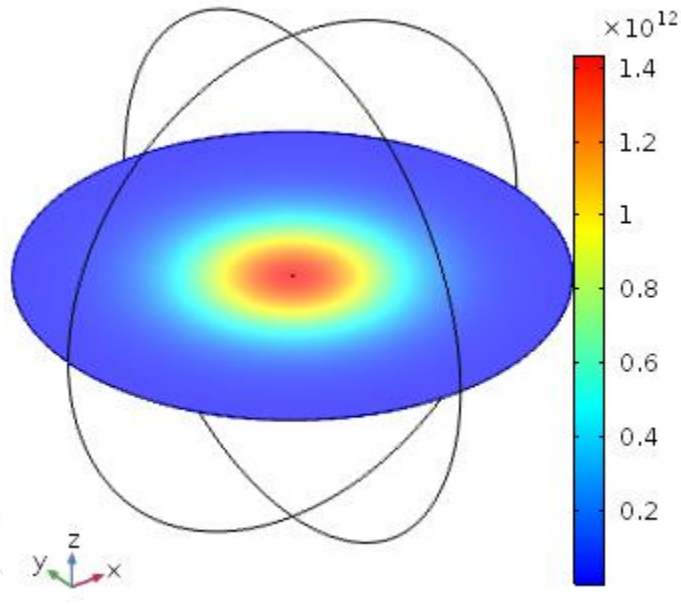
ϵ_a 0 s²/m

Model validation

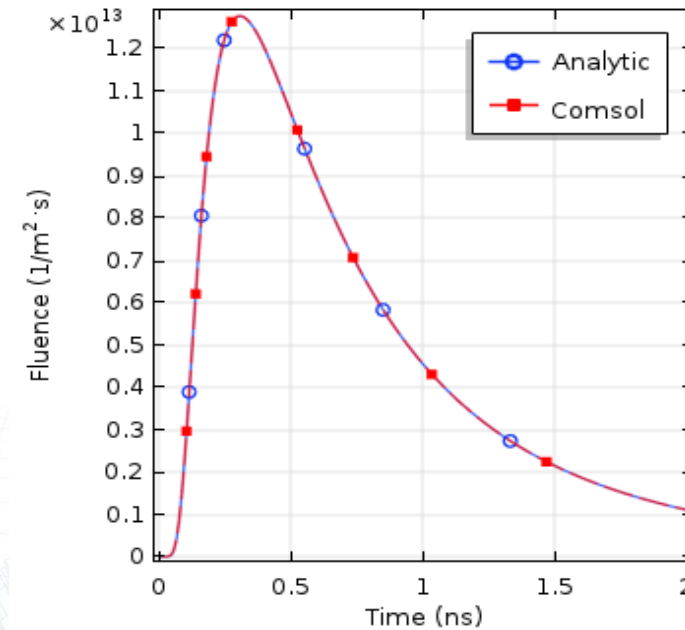
- Light pulse in an infinite homogeneous medium

$$\Phi = c(4\pi Dct)^{-3/2} \exp(-\mu_a ct) \exp\left(\frac{-r^2}{4Dct}\right)$$

Fluence distribution

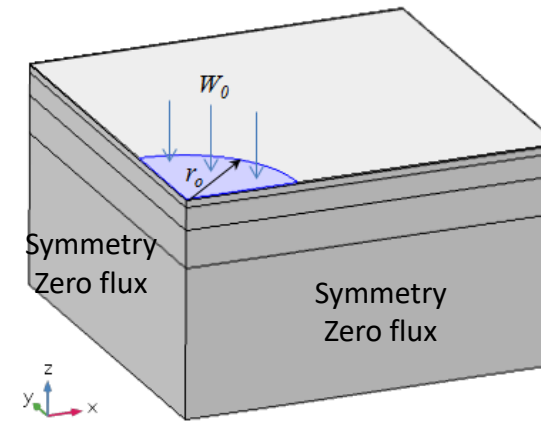
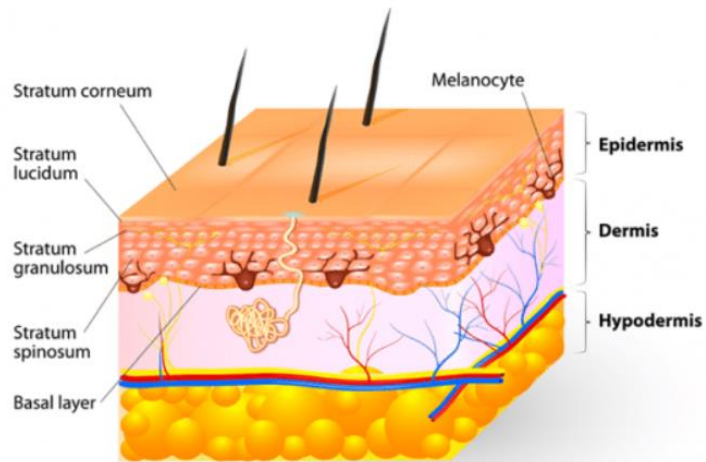


Analytical vs COMSOL



Light diffusion: Tissue

- Simplified layer structure
- Boundary conditions



Fluence continuity
Interior boundaries

Heat transfer: Tissue

- Time dependent tissue temperature due to photon absorption

$$\rho C_p \frac{\partial}{\partial t} T + \nabla \cdot (-k \nabla T) = Q_{light} + Q_{bio}$$

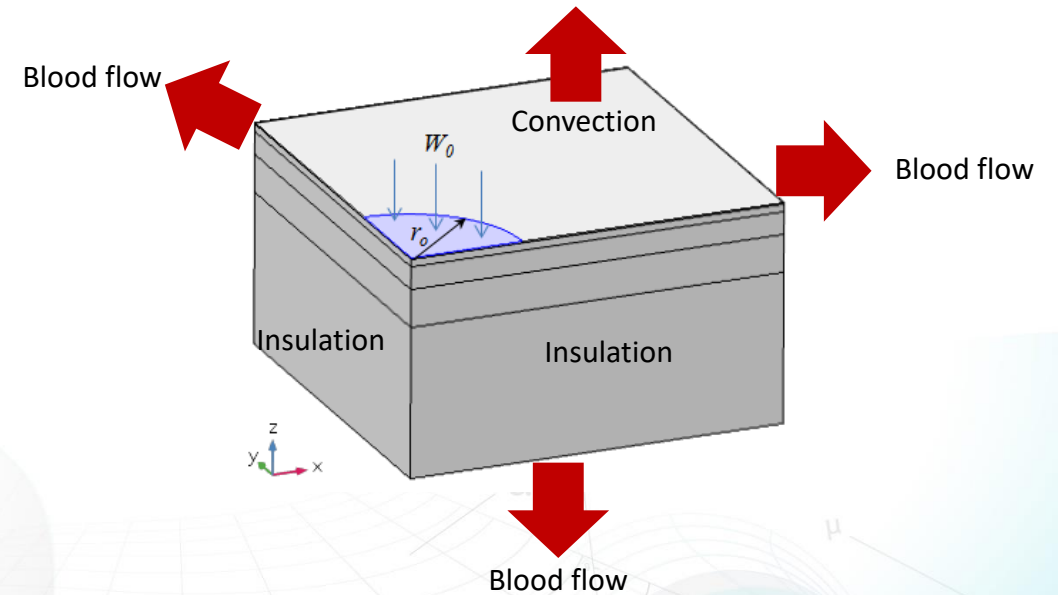
- Heat source due to light

$$Q_{light} = \mu_a \Phi \cdot h(\nu)$$

- Heat transfer due to perfusion

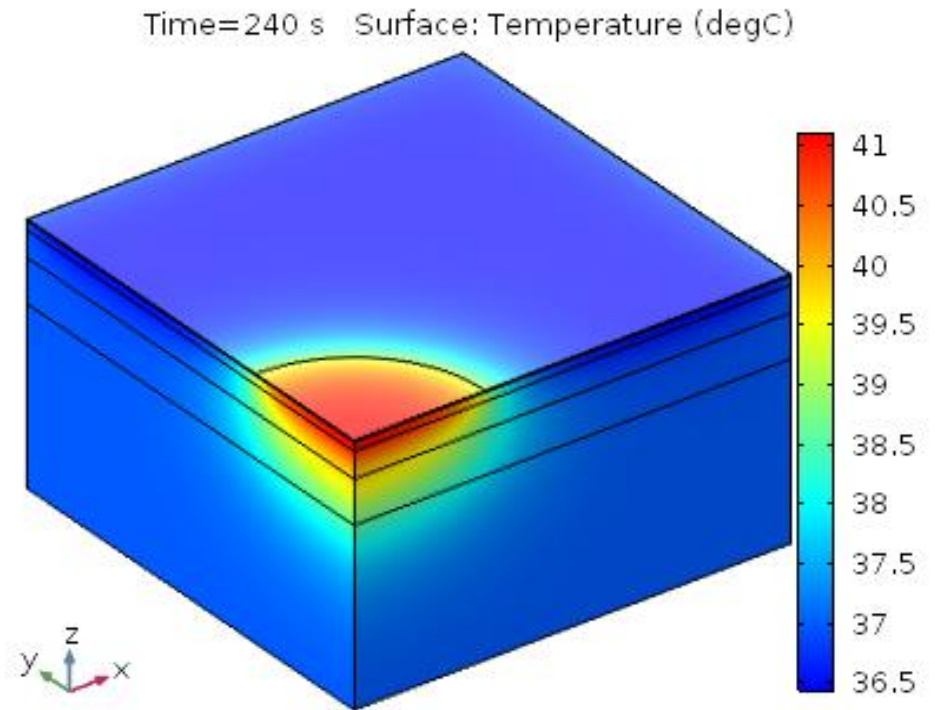
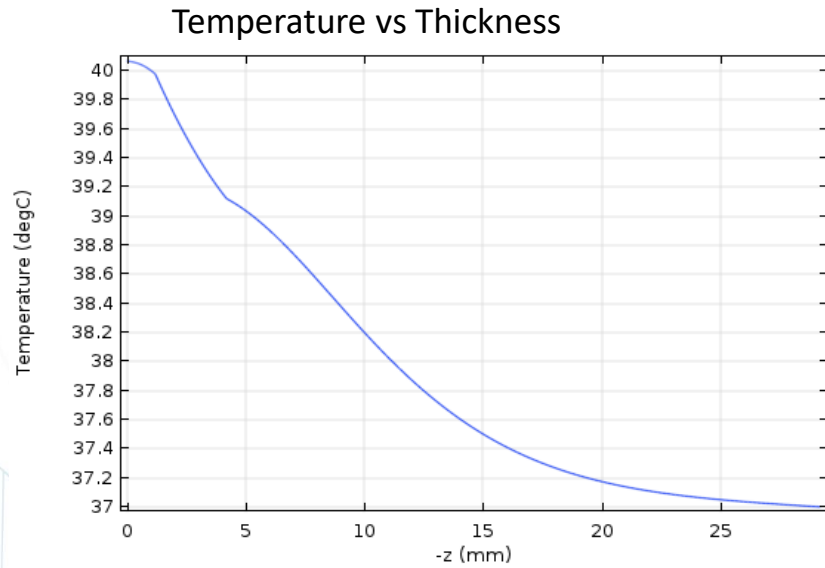
$$Q_{bio} = \rho_b C_{p,b} \omega_b (T - T_b)$$

- Boundary conditions



Tissue heating

- Transient and steady state temperature distribution as a function of laser light parameters



Summary

- Model developed to predict transient temperature response of human tissue when subject to laser radiation
- Thermal history:
 - Laser power
 - Thermal dissipation due to human body
- Optimization of therapeutic patient treatment profiles